

A $0.5\text{ V} < 4\ \mu\text{W}$ CMOS Light-to-Digital Converter Based on a Nonuniform Quantizer for a Photoplethysmographic Heart-Rate Sensor

Mohammad Alhawari, Nadya A. Albelooshi, and Michael H. Perrott, *Senior Member, IEEE*

Abstract—A 0.5 V CMOS light-to-digital converter (LDC) based on a nonuniform quantizer and off-chip photodiode enables a photodiode bias current (I_{bias}) range spanning 4 nA to $3.5\ \mu\text{A}$ while consuming less than $4\ \mu\text{W}$ of power. Using an off-chip LED as a modulated light source, measurements with a photodiode current signal having modulation frequency of 1.2 Hz (72 beats per minute) and 0.5% peak-to-peak amplitude relative to I_{bias} performed at the low and high end of the I_{bias} range confirm over 30 dB of SNR for an integration bandwidth spanning 0.5 to 5 Hz . Using off-chip digital signal processing of the LDC output, instantaneous period jitter (a proxy for instantaneous heart rate) is measured to be less than 0.45% (rms) of the period, and the high sensitivity of the LDC allows detection of the heart-rate signal from a finger pressed against the off-chip photodiode using only ambient light. Key circuit components of the LDC include a wide range logarithmic digital-to-resistance converter (DRC) utilizing digital multibit $\Delta\Sigma$ modulation to achieve fine resolution and a nonuniform quantizer based on a ladder inverter quantizer (LIQAF) which also acts as a low-noise front-end amplifier and filter.

Index Terms—Analog-to-digital converter (ADC), Delta-Sigma, digital-to-resistance converter (DRC), heart-rate sensor, ladder inverter, light sensor, ladder inverter quantizer/amplifier/filter (LIQAF), low-noise amplifier, nonuniform quantizer, photodetector, photoplethysmographic, resistor DAC, oximetry.

I. INTRODUCTION

HEART rate is a key vital sign to assess the health of an individual and is routinely monitored within clinical settings using pulse oximetry or EKG instruments. Unfortunately, for most individuals, the clinical setting is the only place where their heart rate is observed, which leads to long time durations in which this important vital sign is largely ignored. This issue has been addressed within the context of athletic activities with the advent of sport watches which measure heart rate using chest straps, contact electrodes, and photoplethysmographic methods as used in pulse oximetry devices. However, thus far there has

Manuscript received April 17, 2013; revised August 24, 2013; accepted August 27, 2013. Date of publication October 21, 2013; date of current version December 20, 2013. This paper was approved by Guest Editor Michiel Pertijs.

M. Alhawari was with the Masdar Institute of Science and Technology, Abu Dhabi, UAE. He is now with Khalifa University, Abu Dhabi, UAE.

N. A. Albelooshi was with the Masdar Institute of Science and Technology, Abu Dhabi, UAE. She is now with Abu Dhabi Company for Onshore Oil Operations (ADCO), Abu Dhabi, UAE.

M. H. Perrott was with the Masdar Institute of Science and Technology, Abu Dhabi, UAE. He is now with Silicon Laboratories, Nashua, NH 03062 USA.

Color versions of one or more of the figures in this paper are available online at <http://ieeexplore.ieee.org>.

Digital Object Identifier 10.1109/JSSC.2013.2284349

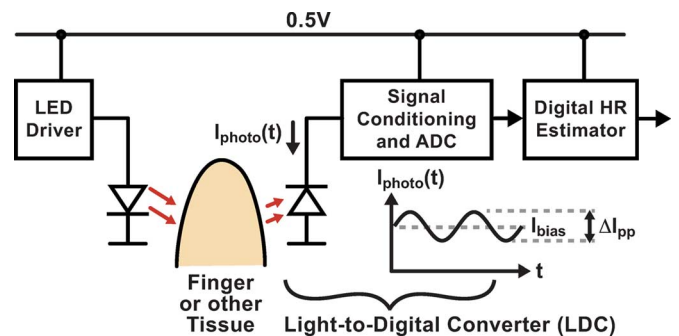


Fig. 1. Overview of heart-rate sensor based on measurement of light fluctuations due to pulsed blood flow through tissue such as a finger.

been very limited impact of such heart-rate monitor devices on the general public due to issues such as their relatively high cost and inconvenient form factor.

In this paper, we present a light-to-digital converter (LDC) for photoplethysmographic-based heart-rate monitoring which achieves high sensitivity and wide dynamic range while consuming very low power and operating with a low supply voltage. As illustrated in Fig. 1, the LDC circuit, which utilizes an off-chip photodiode, acts as the front-end of an overall system which includes an off-chip LED, an LED driver operating from a 0.5-V supply voltage [1], and digital signal processing to estimate heart rate. The heart-rate signal is sensed as fluctuations in light intensity as the light passes through tissue such as a finger, with the photodiode generating a current $I_{\text{photo}}(t)$ proportional to the light intensity. The peak-to-peak amplitude in photodiode current ΔI_{pp} is typically in the range of 0.5% to 2% of its bias current I_{bias} [2]. In general, it is highly desirable to achieve high sensitivity by being able to sense the signal at low values of I_{bias} , and to support a wide dynamic range (i.e., a large ratio of maximum to minimum I_{bias}).

Within the overall system in Fig. 1, the LDC is the key circuit for achieving high sensitivity and wide dynamic range. Low-power operation is critical in order to achieve a small form factor by minimizing the size of the energy storage device. A low supply voltage of 0.5 V potentially enables a simple energy-harvesting approach consisting of a direct connection to a solar cell that operates at such voltage levels. Using an LED as the light source leads to the LED driver becoming the dominant power consumer in the system, but improved sensitivity in the LDC reduces the light intensity required from the LED (since lower photodetector current becomes acceptable) and, therefore, lowers the power of the LED driver. The preferred

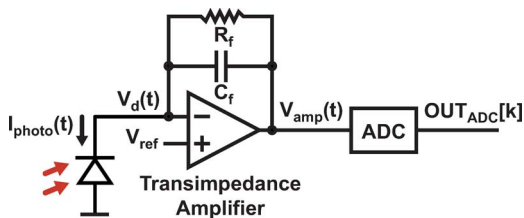


Fig. 2. Classical LDC consisting of a transimpedance amplifier and ADC.

operating mode is to avoid powering the LED light source and instead use ambient light, which, as shown in Section V, may be possible for some applications due to the high sensitivity of the proposed LDC.

To highlight the key challenges in achieving the desired performance characteristics of the LDC, consider the classical implementation shown in Fig. 2. Here, a transimpedance amplifier is utilized to convert the photodiode current, $I_{\text{photo}}(t)$, to a voltage, $V_{\text{amp}}(t)$, which is then converted to a digital representation by an analog-to-digital converter (ADC). In this structure, the feedback action of the transimpedance amplifier maintains a constant photodiode voltage $V_d(t)$ and provides a low impedance to the photodiode such that $I_{\text{photo}}(t)$ is shunted through an RC feedback network consisting of R_f and C_f . The conversion gain from current $I_{\text{photo}}(t)$ to voltage $V_{\text{amp}}(t)$ is set by the value of R_f , and low-pass filtering is provided by including C_f in order to reduce the impact of noise and 50/60 Hz power line corruption. Note that, for heart-rate monitoring, the signal bandwidth typically spans from 0.5 to 5 Hz, which corresponds to 30–300 beats per minute (bpm), respectively.

To achieve high sensitivity, the opamp shown in Fig. 2 must be designed to have adequately low $1/f$ and thermal noise, the ADC must have adequate resolution, and the RC filtering must attenuate noise above 5 Hz, with reduction of 50/60 Hz power line corruption being of particular concern. The large dc operating range required of the ADC complicates its design, and achievement of <5 Hz bandwidth with on-chip RC elements is quite challenging when seeking a low area solution.

To achieve wide dynamic range, the feedback resistor R_f can be made adjustable as is commonly done in variable gain amplifiers (VGA) [3]. However, if one uses a typical VGA approach of utilizing a switched resistor network for variable R_f , it leads to discrete operating regions. Unfortunately, operation across such regions leads to large perturbations of $I_{\text{photo}}(t)$ and loss of information due to the discrete nature of the gain switching and its associated transient effects.

In contrast to the classical approach discussed above, we propose the LDC structure shown in Fig. 3. Rather than cascading the transimpedance amplifier with the ADC, the proposed structure combines these functions within a single closed-loop feedback structure. In this design, the traditional transimpedance amplifier is replaced by a digital-to-resistance converter (DRC) consisting of a logarithmic resistor network and digital multibit $\Delta\Sigma$ modulator. A parallel resistor, R_{par} , improves sensitivity and dynamic range by extending the minimum value of I_{bias} that is supported. The combination of the DRC and R_{par} enable continuous operation of the LDC over approximately three orders of magnitude range of I_{bias} . The DRC is controlled through

feedback which consists of a digital accumulator and nonuniform quantizer based on a ladder inverter quantizer/amplifier/filter (LIQAF) [4], which eliminates the need for external passive components such as filter capacitors. The DRC value is set such that the photodiode voltage, $V_d(t)$, matches the desired operating point of an inverter-based low-noise amplifier (LNA) that is realized by the LIQAF-based quantizer. The inverter-based LNA structure provides an efficient means of achieving good noise performance since it minimizes the number of devices that contribute noise and uses the same current for both NMOS and PMOS transistor devices [5].

Closer inspection of Fig. 3 reveals that the proposed LDC structure is similar to a Delta modulator [6]–[9], but utilizes a multibit, nonuniform quantizer and digital accumulator. In contrast to $\Delta\Sigma$ modulators, the noise of the quantizer is not shaped for Delta modulators. However, $\Delta\Sigma$ modulators require analog integration before the quantizer, which leads to challenges in achieving high dc gain, low area, and low power consumption. The advantage of the proposed structure is that the fine resolution region of the LIQAF-based quantizer offers low quantization noise (under the assumptions discussed below) and the digital accumulator provides the desired characteristics of low area and low power consumption compared with using an analog integrator. The digital accumulator also provides infinite dc gain, which is seen by examining its Z -transform as frequency f goes to 0:

$$\lim_{f \rightarrow 0} \left. \frac{K_{\text{accum}}}{1 - z^{-1}} \right|_{z = e^{j2\pi f T_{\text{clk}}}} = \infty \quad (1)$$

where $T_{\text{clk}} = 1/32$ kHz represents the time step of the accumulator and K_{accum} is a scale factor which is set to achieve the desired closed loop bandwidth of the LDC. The infinite dc gain of the accumulator allows perfect centering of the nonuniform quantizer during steady-state operation such that, assuming small perturbations to the system, the fine quantization region is utilized to achieve low quantization noise. In the case of large perturbations, the wide range of the nonuniform quantizer characteristic offers a high slew rate which benefits the tracking performance of the LDC.

In practice, the steady-state behavior of the LDC dynamics will vary according to the influence of input stimulus and noise on the nonuniform quantizer. Assuming small input stimulus and noise such that saturation effects are avoided in the quantizer, but sufficiently large stimulus and/or noise to cause sufficient scrambling activity in the quantizer, the LDC feedback dynamics can be approximated as having linear behavior. In such a case, moderate levels of quantizer mismatch will have only a minor impact on LDC distortion performance since the quantizer sees only the *residual error* of the feedback loop which, in turn, is suppressed by the open-loop gain of the accumulator. However, for cases where the input stimulus is sufficiently large to cause saturation effects in the quantizer, slew-rate-limited behavior occurs in the LDC that can cause significant distortion. For the proposed heart-rate (HR) detection application, such distortion is acceptable assuming that the desired information corresponds to the time between edges of the HR signal and that the HR signal is significantly larger than interfering signals (such as 50/60 Hz power line corruption). Given such assumptions,

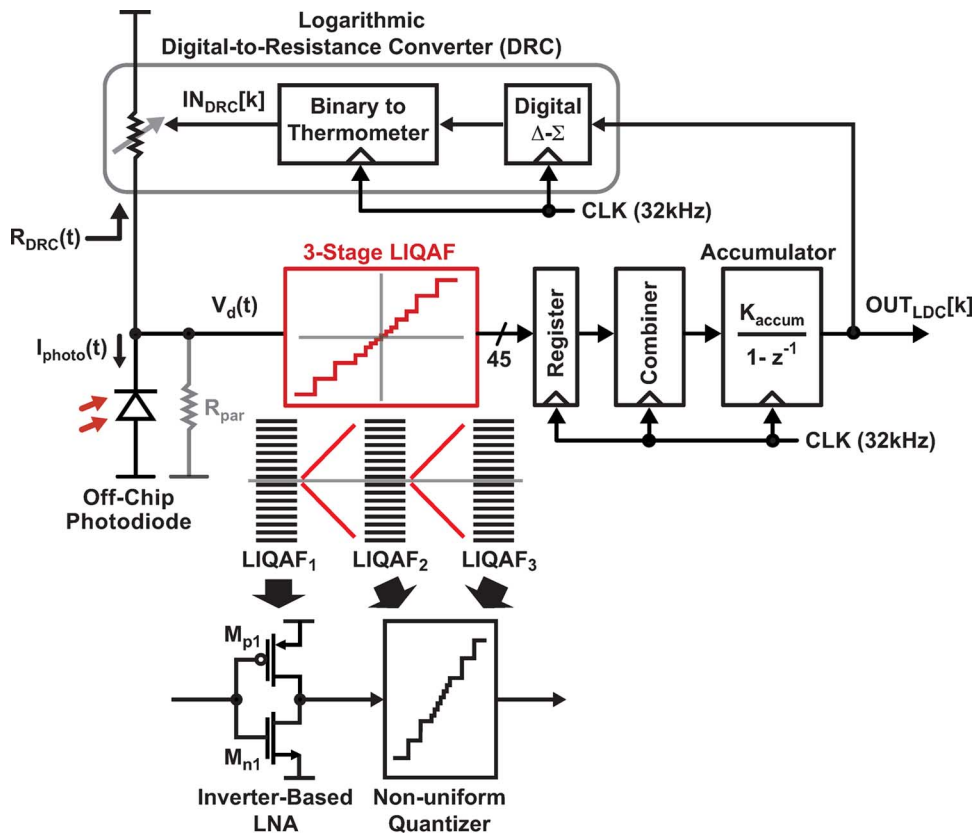


Fig. 3. Proposed LDC architecture.

SNR rather than SNDR is considered to be the key performance metric for this application.

The remainder of this paper is organized as follows. Section II covers additional background information on previous circuit approaches developed for LDC structures. Section III then presents details of the proposed LDC circuits, with primary focus being placed on the DRC and nonuniform LIQAF-based quantizer. Section IV provides high-level system and noise analysis, and Section V presents measured results from a prototype IC. Finally, Section VI concludes.

II. BACKGROUND

Prior work on improving the performance of LDC circuits is illustrated in Fig. 4. As indicated in Fig. 4(a), improved dynamic range was pursued by rejecting the dc bias of the photodiode current through the use of an auxiliary feedback amplifier and photodiode bias circuit [10]–[12]. However, the additional circuitry in this approach adds noise, thereby reducing sensitivity, and the resulting ac coupling of the photodiode current signal causes a significant increase in settling time when large perturbations are encountered. A dc-coupled solution to improving dynamic range is shown in Fig. 4(b), in which the logarithmic current-to-voltage characteristic of an NMOS device in the sub-threshold region is utilized to allow a wide range of photodiode current without saturating the transimpedance amplifier [13]. A key issue of concern in this design is that the reduced transimpedance gain of the logarithmic current-to-voltage characteristic can lead to reduced sensitivity due to the higher impact

of opamp noise. Finally, a closed-loop approach combining the transimpedance amplifier and ADC is shown in Fig. 4(c) [14]. Here, a switched capacitor network provides current to the photodiode in order to maintain the photodiode voltage $V_d(t)$ at a constant value. This technique allows a simple quantizer to be used for digitizing the signal, but the issue of achieving wide dynamic range was not addressed in this work.

III. PROPOSED LDC ARCHITECTURE

The proposed system shown in Fig. 3 combines the ideas of Fig. 4(b) and (c) by utilizing a logarithmic current-to-voltage characteristic in combination with a closed-loop feedback topology that provides digitization of the signal. However, in contrast to the previous approaches, the proposed system offers a highly digital implementation that minimizes analog complexity. Further, as we will show later in this paper, the design enables wide dynamic range and high sensitivity to be achieved with low-voltage and low-power operation.

Further examination of Fig. 3 reveals two key circuits that enable the highly digital LDC implementation while achieving high performance. The first circuit is the DRC mentioned earlier, in which a digital $\Delta\Sigma$ modulator dithers switches connected to a resistor network in order to achieve high-resolution control of resistance across a wide range. The second circuit is a nonuniform LIQAF-based quantizer that provides an efficient approach to realizing the inverter-based LNA and nonuniform quantizer as depicted in Fig. 3. Each of these circuits will be discussed in further detail in the subsections to follow.

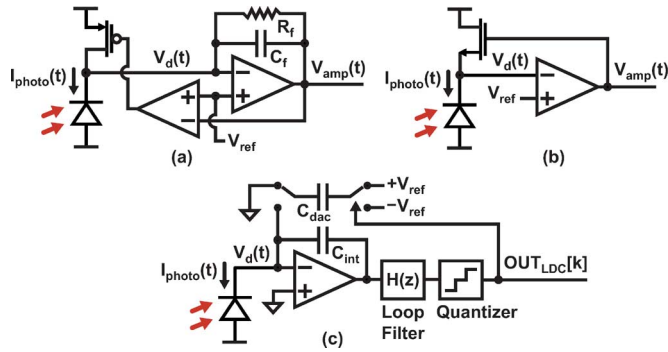


Fig. 4. Prior circuit topologies for improving the performance of LDC circuits. (a) Attenuation of dc offset using feedback [10]–[12]. (b) Improved dynamic range using the logarithmic characteristic of a subthreshold NMOS device [13]. (c) Switched-capacitor-based closed-loop feedback design [14].

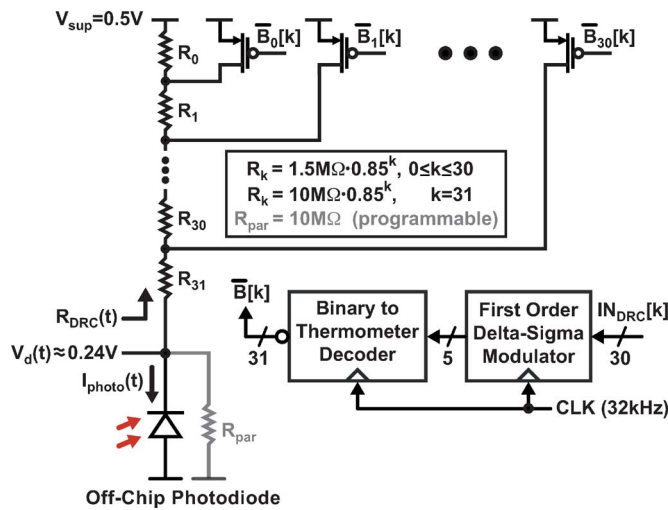


Fig. 5. Logarithmic DRC.

A. Digital-to-Resistance Converter

Fig. 5 provides a more detailed view of the DRC circuit. The variable resistance $R_{DRC}(t)$ is achieved with a set of PMOS switches connected to taps of a polysilicon resistor string ladder, with the PMOS switches being controlled by the output of a digital $\Delta\Sigma$ modulator that provides high-resolution resistance control through dithering.

In order to achieve a wide range of resistance values, the resistor elements within the ladder are progressively scaled according to the equation given in the figure. The maximum resistance, which occurs when all switches are open, corresponds to the sum of all resistor legs which yields $R_{DRC} = 10 M\Omega$. The minimum resistance, which occurs when all switches are closed, corresponds to the resistor leg R_{31} which yields $R_{DRC} = 64.9 k\Omega$. As such, R_{DRC} can be varied by more than two orders of magnitude using only 32 resistor elements.

Due to the nonlinearity of the resistor leg values, the multibit digital $\Delta\Sigma$ modulator is chosen to be first order in order to avoid noise folding. To explain, a first order multibit $\Delta\Sigma$ modulator only dithers one switch setting at a time such that the dithering operation does not see the nonlinearity caused by unequal resistor element values. In contrast, a higher order multibit $\Delta\Sigma$ modulator would dither between several switch settings and

thereby expose the $\Delta\Sigma$ to the nonlinearity of the individual resistor element values. Fortunately, the oversampling ratio is quite high given the clock frequency of 32 kHz versus the desired signal bandwidth of < 5 Hz, so that first-order noise shaping is adequate for this application.

As indicated in Fig. 5, the closed-loop feedback dynamics of the LDC maintain a relatively constant photodiode bias voltage $V_d(t)$ such that the LIQAF-based nonuniform quantizer is centered in its fine quantization region. To simplify the analysis to follow, we will assume $V_d(t) \approx 0.24$ V under nominal conditions for a 0.5-V supply. Given this assumption, the minimum current supported by the $R_{DRC}(t)$ ladder is 26 nA (i.e., $(0.5 V - 0.24 V)/10 M\Omega$). In order to improve sensitivity, a parallel resistor R_{par} is connected which reduces the minimum photodiode current that is supported. R_{par} is made programmable using on-chip poly resistors and NMOS switches in order to accommodate variation in $V_d(t)$ away from its assumed 0.24-V bias value. As discussed in Section IV, the presence of R_{par} provides substantial improvement to the dynamic range of the LDC at a slight cost to SNR.

B. Laddered-Inverter Quantizer/Amplifier/Filter

To gain an understanding of the LIQAF circuit, consider the simplified structure shown in Fig. 6(a) in which only two output levels are implemented. As indicated in Fig. 6(b), we can view this circuit as a combination of two CMOS inverters that have different ratios of NMOS versus PMOS gate lengths, which yields the shifted dc characteristics shown in the figure. To explain, note that, when V_{in} is low and both outputs are high, transistor M_1 is inactive such that V_{out0} transitions with increasing V_{in} according to a CMOS inverter characteristic with one NMOS device and two series PMOS devices. In contrast, when V_{in} is high and both outputs are low, M_2 is inactive such that V_{out1} transitions with decreasing V_{in} according to a CMOS inverter characteristic with two series NMOS devices and one PMOS device. Since V_{out0} cannot transition high unless V_{out1} is also high, and V_{out1} cannot transition low unless V_{out0} is also low, the LIQAF circuit provides guaranteed monotonicity in the quantizer characteristic regardless of the presence of mismatch. Note that one should not confuse the curves shown in Fig. 6(a) with the phenomenon of hysteresis—they instead correspond to the dc characteristic of the structure that is independent of the previous state of the input. As will soon be discussed, a very useful aspect of the LIQAF circuit is that it can be utilized as an inverter-based LNA when operating at the mid-rail voltage of a given output (i.e., halfway between supply voltage and ground). Finally, note that the same current is shared by all of the devices, which aids in achieving low power consumption.

In order to increase the number of quantization levels, the prototype LDC presented in this paper makes use of a 15-output LIQAF structure. Fig. 7 depicts the extension of Fig. 6(a) to achieve the increased number of outputs, and also shows simulated dc characteristics for each output as the supply voltage is varied from 0.5 to 1.8 Volts, with the preferred voltage in this application being 0.5 V. The simulated dc characteristics reveal that the quantization behavior is robust across a large supply range. Based on similar arguments as made for the two-output LIQAF example, the quantizer levels are guaranteed to

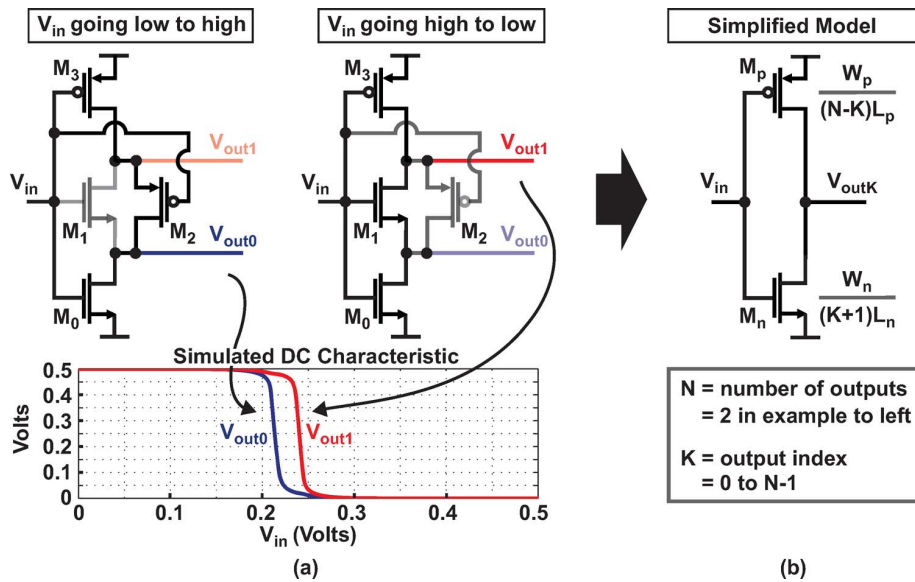


Fig. 6. Basic principles of a two-output LIQAF circuit. (a) Circuit and simulated dc characteristic. (b) Simplified model.

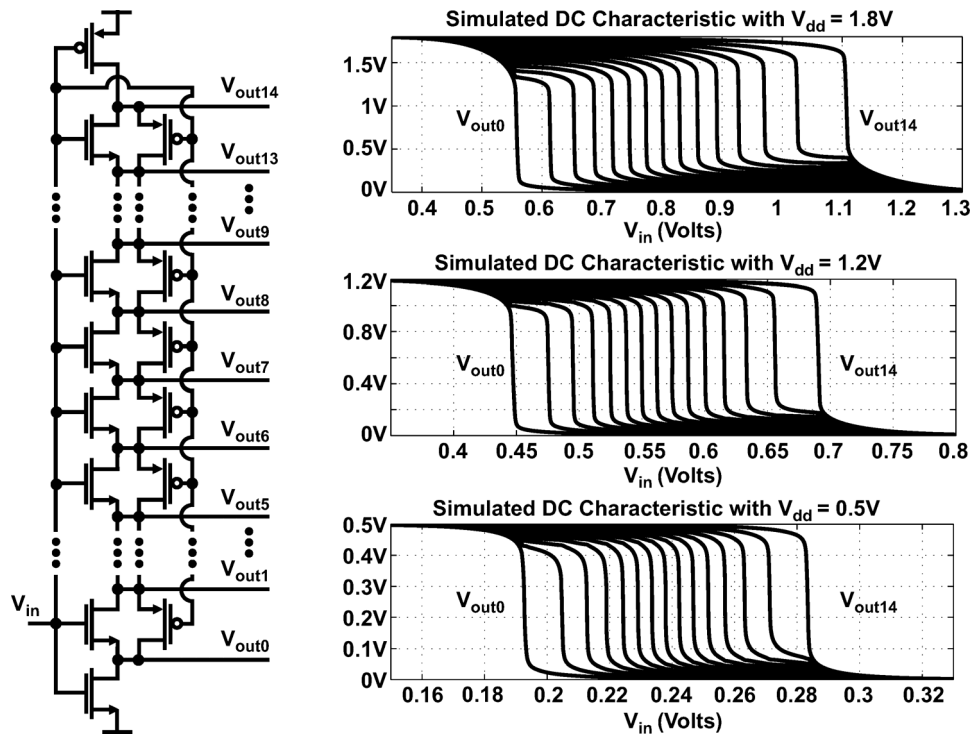


Fig. 7. The 15-output LIQAF circuit along with its simulated dc characteristic under different supply voltages.

be monotonic regardless of the impact of mismatch. To further elaborate, let us define $V_{in(K)}$ as the input voltage such that output voltage $V_{out(K)}$ is at its mid-rail value. Since a given output voltage $V_{out(K)}$ must be strictly larger than $V_{out(K-1)}$ and strictly lower than $V_{out(K+1)}$, we see that $V_{in(K)}$ must have a value strictly *between* $V_{in(K-1)}$ and $V_{in(K+1)}$.

With the increase in number of quantizer outputs in Fig. 7, large output resistance is encountered due to the large effective gate length of the respective inverter structures. Large output resistance leads to low bandwidth and relatively high intrinsic gain (i.e., $g_m r_o$) when a given inverter is in its transition

region. Fortunately, the low bandwidth is an asset to the given LDC application since it provides rejection of undesired noise. However, when using the V_{out7} output as the input to the next LIQAF stage, lower gain is desirable to avoid overly reducing the range of the medium and high resolution quantizer regions (as soon discussed). To address this issue, a transistor-based load is added to the LIQAF V_{out7} output, along with its closest neighbors, as shown in Fig. 8. As seen in the measured dc characteristic depicted in the figure, the presence of the load leads to a reduced slope over the key portion of the V_{out7} transition region impacting the LIQAF stage to follow.

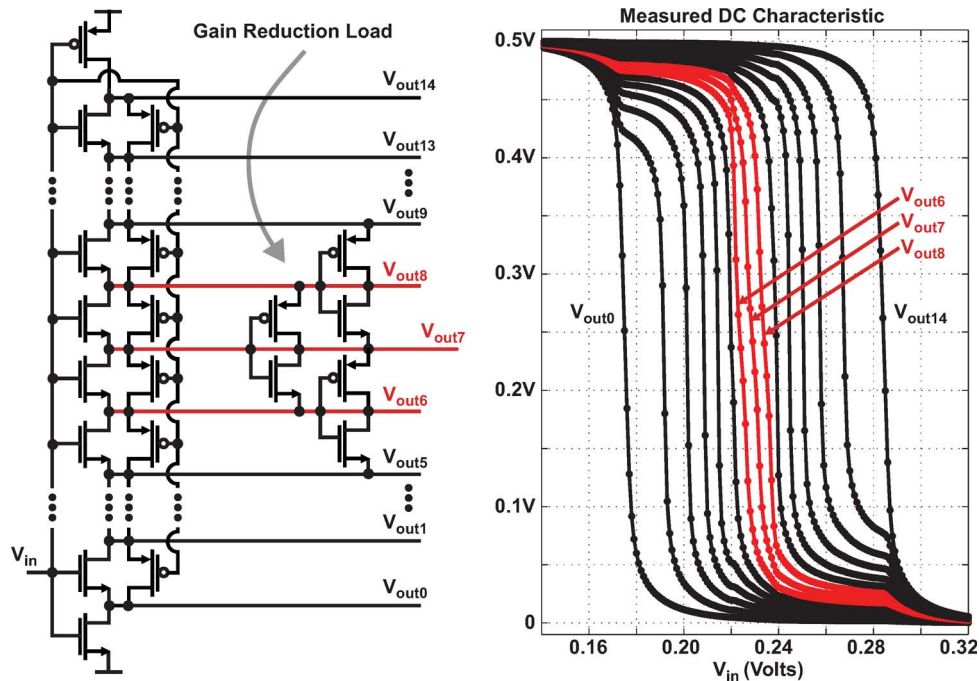


Fig. 8. A 15-output LIQAF circuit with gain reduction load on V_{out7} (which is passed to the following LIQAF stage) along with its measured dc characteristic from the custom IC.

The overall three-stage LIQAF-based quantizer structure, along with its measured dc characteristic, is shown in Fig. 9. The quantizer characteristic reveals progressively improved resolution as the input voltage is swept from coarse to fine regions, with a center voltage at approximately 0.235 V based on a supply voltage of 0.5 V. While more LIQAF stages could be added to achieve even finer resolution, Section IV reveals that this three-stage design achieves an adequately small step size in its fine resolution region such that the fine range quantization noise does not set the bottleneck in the overall LDC noise performance.

To better understand the role of the cascaded stages in forming the nonuniform quantizer characteristic, Fig. 10 provides an intuitive look at how signal amplitude at the input of LIQAF₁, operating as an LNA, activates the various quantization levels of LIQAF₂, operating as a quantizer. It should be observed that the quantizer range of LIQAF₂ is referred to the input of LIQAF₁ according to the dc characteristic of output V_{out7} of LIQAF₁, with dc gain at the mid level of V_{out7} serving as an approximate metric to evaluate this relationship. One should note that excessively large dc gain leads to an unnecessarily reduced LIQAF₂ quantizer range when referred to the LIQAF₁ input, which is undesirable since it limits the input range of the cascaded quantizer over which smaller quantization steps are available. This observation helps to clarify the benefit of using the dc gain reduction load on the LIQAF structure shown in Fig. 8.

Fig. 10 also indicates that achievement of monotonicity for the cascaded LIQAF stages requires that the input-referred quantizer range of LIQAF₂ be contained within the LIQAF₁ quantizer transition boundaries of V_{out6} and V_{out8} . Note that in constructing the cascaded quantizer characteristic with the digital combiner circuit shown in Fig. 9, V_{out7} of LIQAF₁ and

LIQAF₂ are ignored such that outputs V_{out6} and V_{out8} provide the nearest LIQAF₁ quantization levels when operating LIQAF₁ as an LNA. For the given prototype, the measured quantizer characteristic in Fig. 9 indicates that the above monotonicity condition is clearly met.

Process, voltage, and temperature (PVT) variations will alter the LIQAF characteristics as it operates as either an LNA or quantizer. Focusing first on the LNA-related issues of dc gain and bandwidth, Fig. 11 shows the SPICE simulated frequency response at the mid-rail output level for V_{out7} on LIQAF₁ and LIQAF₂ under PVT variations, which reveal less than 4-dB midpoint dc gain variation but significant bandwidth variation. Fortunately, the bandwidth stays well above the <5-Hz closed-loop bandwidth of the LDC, so that its impact on stability of the closed-loop dynamics of the LDC is minimal. As indicated in Fig. 11, LIQAF₁ is sized to be much larger than LIQAF₂ in order to reduce the impact of $1/f$ noise.

To investigate quantizer-related issues, Fig. 12 shows the worse case SPICE simulated dc characteristics of LIQAF₁ and LIQAF₂ under PVT variations in terms of minimum and maximum input range. Fortunately, the overall quantizer behavior appears robust. The key characteristics to consider for the LIQAF-based quantizer under PVT variations are its offset, gain, and filtering characteristic. Variations in offset are accommodated by the infinite dc gain of the accumulator within the LDC, which ensures that the steady-state input into the cascaded quantizer centers it within its fine quantization region. The impact of the resulting shift of the bias voltage (i.e., $V_d(t)$) on I_{bias} can be somewhat mitigated by adjusting the value of R_{par} such that the LDC sensitivity is maintained. Variations in gain correspondingly change the open loop gain of the LDC, which results in variation of the closed loop bandwidth of the LDC. To avoid stability issues

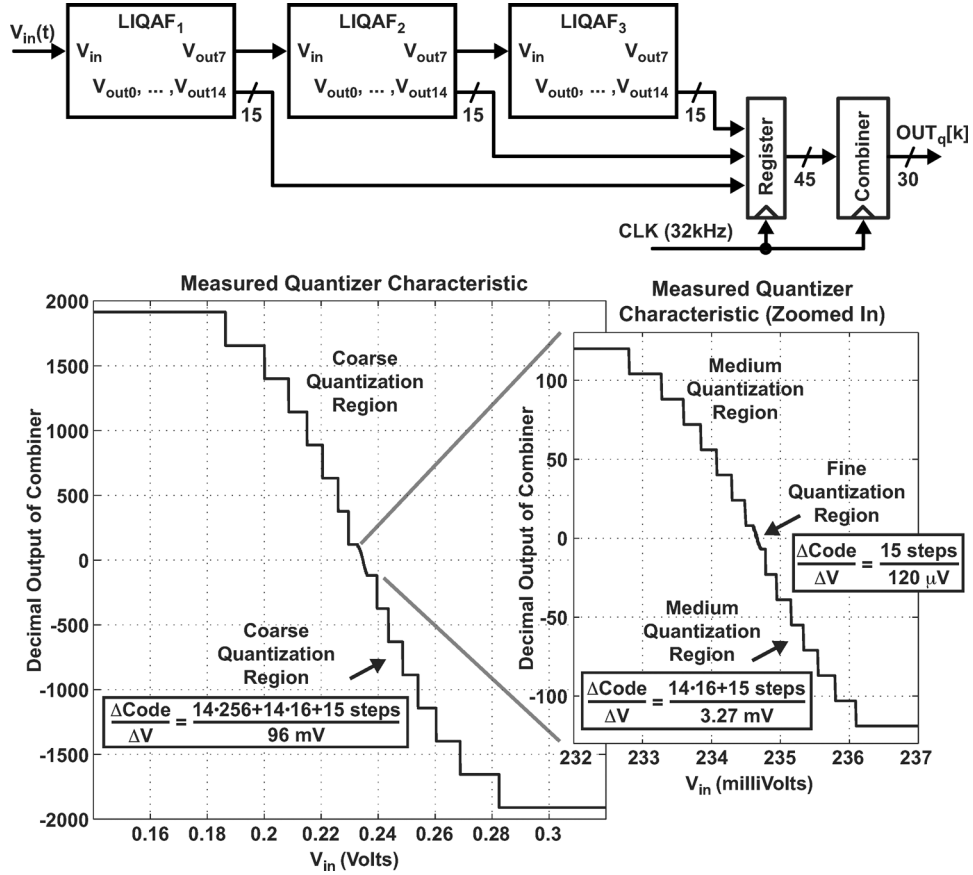


Fig. 9. Three-stage LIQAF quantizer along with its measured quantizer characteristic from the custom IC.

in such case, the poles of the LIQAF LNA/quantizer, which form the filter responses shown in Fig. 11, should be designed to be sufficiently high relative to the closed loop bandwidth of the LDC. This condition must also be met for the pole of the front-end filter, which corresponds to the RC lowpass transfer function from $I_{\text{photo}}(t)$ to $V_d(t)$ formed by the DRC/ R_{par} resistance and photodiode/LIQAF input capacitance. Finally, variations in the filtering characteristic of the LIQAF circuit, as shown in Fig. 11, can lead to reduced attenuation of the DRC shaped quantization noise, which could overly increase activity in the nonuniform quantizer such that saturation effects are more likely to occur. Fortunately, the front-end filter also helps to attenuate such noise, particularly at low I_{bias} where LDC sensitivity is determined since the lowest front-end filter bandwidth (i.e., highest value of R_{load}) occurs there.

IV. SYSTEM ANALYSIS

We now present modeling of the overall LDC topology with the goal of calculating its achievable SNR performance. We begin by further analyzing the DRC in terms of its gain and the range of I_{bias} that it supports. The focus then turns to analysis of front-end noise sources which include photodiode shot noise, DRC thermal noise, and LIQAF thermal and $1/f$ noise. Finally, we calculate the impact of the LIQAF and $\Delta\Sigma$ quantization noise, and show the theoretically achievable SNR across

the full I_{bias} range of the LDC. For all noise related calculations, we will assume an integration bandwidth of 4.5 Hz spanning from 0.5 to 5 Hz.

A. Analysis of Digital-to-Resistance Converter

The key characteristics of interest for the DRC are its gain and the range of I_{bias} that it supports, which are calculated according to the method shown in part (a) of Fig. 13. As indicated in the figure, this analysis assumes a constant value for the photodiode current, $I_{\text{photo}}(t) \approx I_{\text{bias}}$, at a given DRC setting, where I_{bias} is chosen such that $V_d(t) = V_{\text{bias}}$. The value of V_{bias} , in turn, is set by the feedback of the LDC such that the LIQAF-based quantizer is centered within its fine quantization region. We will assume $V_{\text{bias}} \approx 0.24V$ for the analysis to follow. While PVT variations will alter the value of V_{bias} , as implied by Fig. 12, it is presumed that the value of R_{par} can be adjusted to maintain the LDC sensitivity. Given the above constraint, the DRC code is toggled between adjacent levels for every mid-code level and the resulting voltage deviation, ΔV_{pp} , is calculated. Note that I_{bias} is set according to the midpoint operating point indicated in the figure, and the DRC gain has units of V/step .

The resulting values of DRC gain, K_{DRC} , and photodiode bias current, I_{bias} , versus the midpoint operating points of each DRC code value are shown in parts (b) and (c) of Fig. 13. As a reference point, Fig. 13(b) compares the result of including $R_{\text{par}} = 10 \text{ M}\Omega$ and removing it (i.e., $R_{\text{par}} = \infty$), and confirms that inclusion of R_{par} indeed improves sensitivity by extending

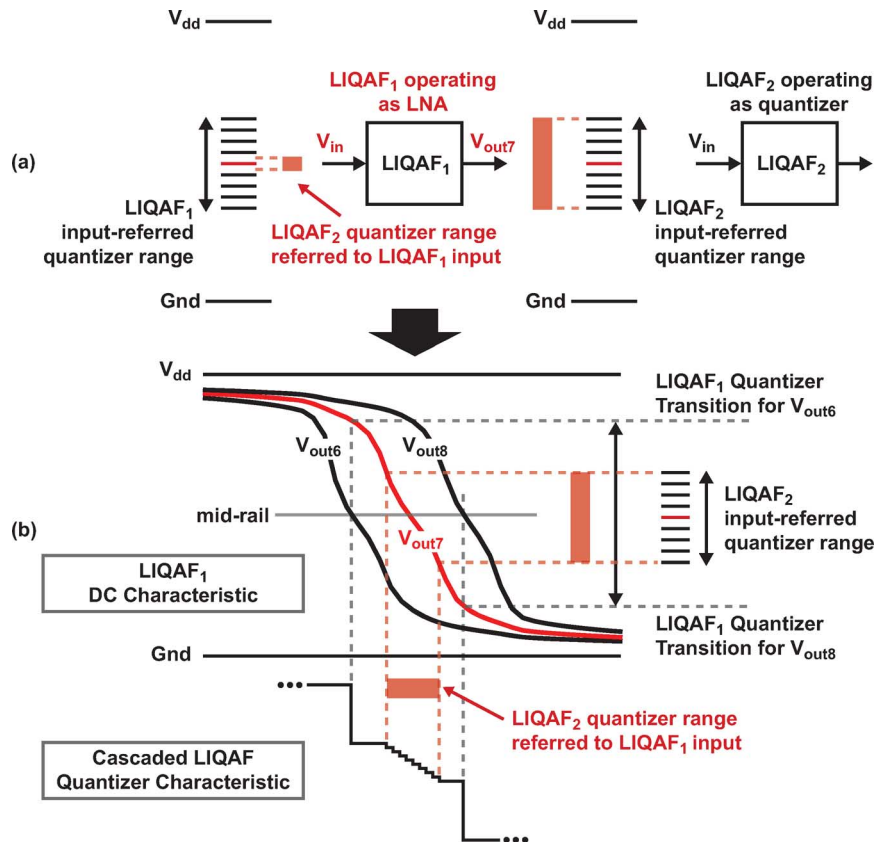


Fig. 10. View of LIQAF₁ as an LNA and LIQAF₂ as a quantizer. (a) Signal amplitude at output of LIQAF₁ compared with range required to activate all quantization levels of LIQAF₂, (b) Comparison of trigger points for quantizer levels above and below V_{out7} of LIQAF₁ to the input-referred quantizer range of LIQAF₂ based on the measured LIQAF dc characteristic.

the minimum supported I_{bias} value to approximately 4 nA. Given the maximum supported I_{bias} value of approximately $3.5 \mu\text{A}$, the dynamic range is roughly three orders of magnitude when including R_{par} .

One consequence of including R_{par} is that it causes DRC gain variation by a factor of two as shown in Fig. 13(c), which directly impacts the open loop gain of the LDC. This gain variation could be reduced by changing the resistor element scaling from what is shown in Fig. 5, but is somewhat balanced out by a counter gain variation in the LIQAF-based nonuniform quantizer as discussed later in this paper.

B. Front-End Noise Analysis

Fig. 14 shows a simplified view of the front-end of the LDC, which includes the photodetector, combined resistance of the DRC and R_{par} , and the LIQAF₁ quantizer along with their noise sources designated as i_{pn}^2 , i_{rn}^2 , and v_{liqafn}^2 , respectively. As depicted in the figure, LIQAF₁ is assumed to be operating as an inverter-based LNA. The signal portion of the photodetector current, $I_{photo}(t)$, is assumed to consist of a bias current, I_{bias} and a sine wave modulation waveform with peak-to-peak amplitude, ΔI_{pp} , and frequency, f_{sig} , such that

$$I_{photo}(t) = I_{bias} + \frac{\Delta I_{pp}}{2} \sin(2\pi f_{sig}t). \quad (2)$$

We will assume that ΔI_{pp} is 0.5% of I_{bias} and that f_{sig} is within the range of 0.5 to 5 Hz.

Single-sided spectral density calculations for each of the front-end noise sources are provided in Fig. 14. In the given formulations, k is the Boltzmann constant, q is the magnitude of charge of an electron, and T_K is temperature in Kelvin. Note that the thermal noise and flicker noise corner (1.3 Hz) of LIQAF₁ operating as an inverter-based LNA were determined from SPICE noise simulations. Also, the impedance of the reverse-biased photodiode is assumed to be much larger than $R_{load}(t)$, and the impact of thermal and flicker noise of LIQAF₂ is assumed to be negligible due to the large gain provided by LIQAF₁.

In order to simplify calculation of the front-end SNR, we ignore the impact of feedback of the LDC other than setting the nominal DRC resistance as a function of I_{bias} such that the LIQAF-based quantizer is centered, which presumably leads to $V_d(t) \approx 0.24 \text{ V}$. Given this assumption, Fig. 15 shows the resulting signal amplitude, rms voltage noise, and SNR as a function of I_{bias} . For reference, the signal amplitude and SNR calculations also include the impact of having R_{par} removed (i.e., having infinite value).

Inspection of Fig. 15(a) leads to a key observation regarding the conversion of the photodetector current signal to the front-end voltage at node $V_d(t)$. Namely, assuming $R_{par} = 10\text{M}\Omega$, the front-end signal swing increases by over an order of magnitude as I_{bias} is increased. When considering the impact of the LDC feedback, the actual front-end signal swing under closed loop conditions will be substantially lower than

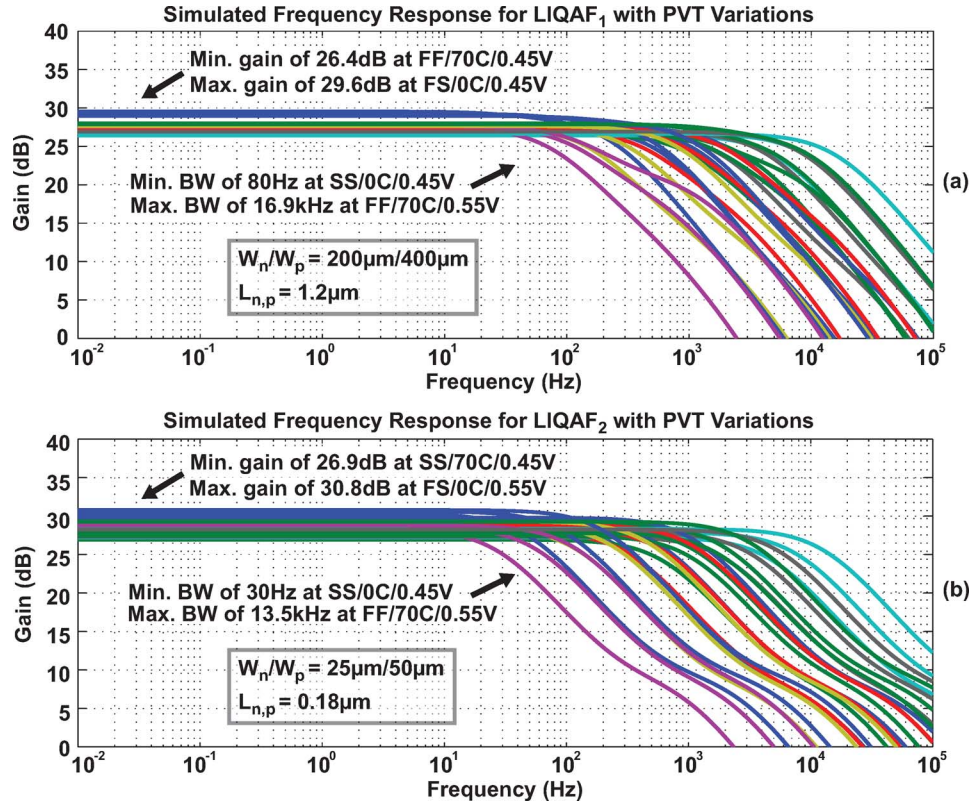


Fig. 11. Simulated frequency responses for (a) LIQAF₁ and (b) LIQAF₂ when operating as an LNA under PVT variations (SS, FS, SF, and FF process, $\pm 10\%$ supply voltage, and 0, 70 °C temperature).

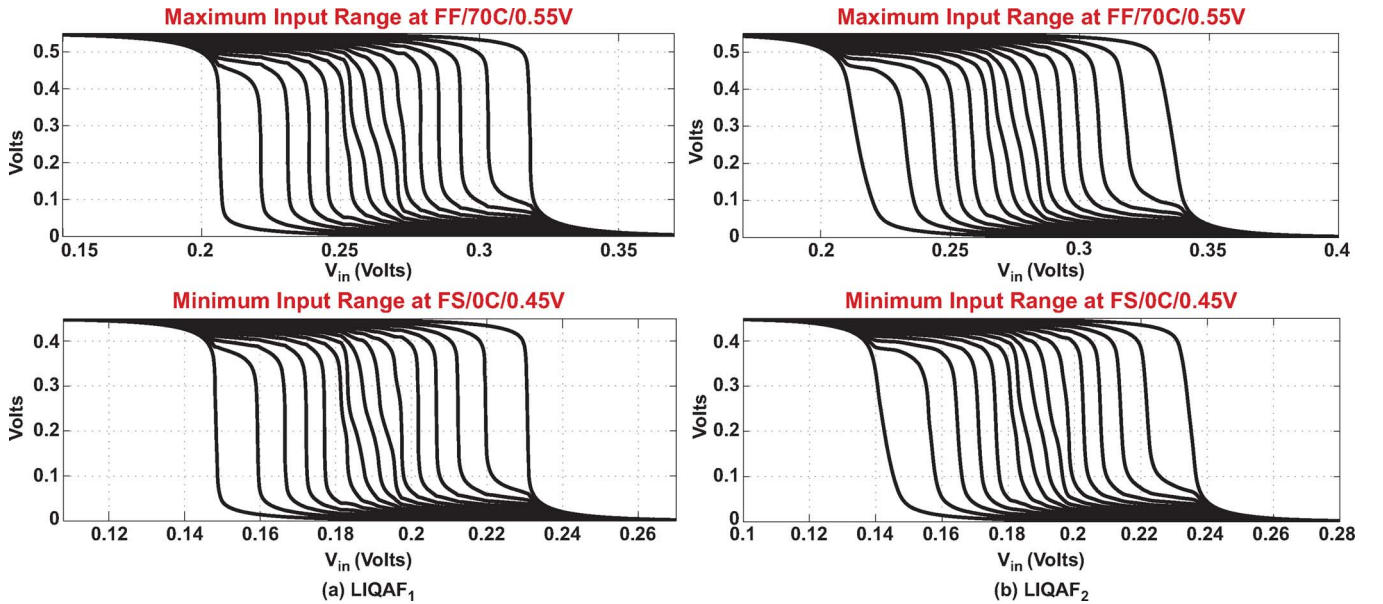


Fig. 12. Simulated worst case PVT corners in terms of minimum and maximum input range for the dc characteristics of (a) LIQAF₁ and (b) LIQAF₂ operating as a quantizer. The worse case PVT corners shown are drawn from simulation results across PVT variations consisting of SS, FS, SF, and FF process, $\pm 10\%$ supply voltage, and 0, 70 °C temperature.

shown in the figure. However, the *relative* increase in signal swing between low and high I_{bias} conditions remains valid, which has implications for the operation of the LIQAF cascaded quantizer as will be discussed in the following subsection. As a point of reference, note that a constant signal swing could be achieved by removing R_{par} at the cost of either reduced range

of I_{bias} or additional control bits and considerably more area for the DRC.

Inspection of Fig. 15(b) leads to several key observations regarding the impact of the various front-end noise sources. First, we observe that the influence of noise from the photodiode and DRC resistor R_{load} decreases with increasing I_{bias} due to the

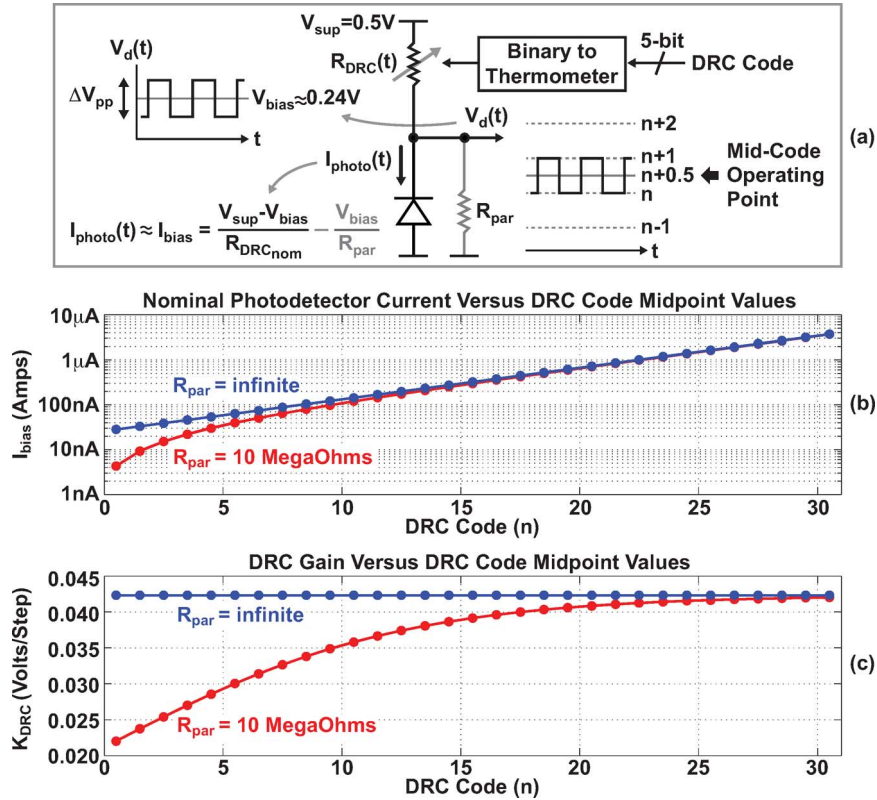


Fig. 13. Simulated plots for DRC within feedback assuming $V_{bias} = 0.24$ V, $V_{sup} = 0.5$ V: (a) characterization approach, (b) supported photodiode bias current versus DRC code, and (c) DRC gain versus DRC code.

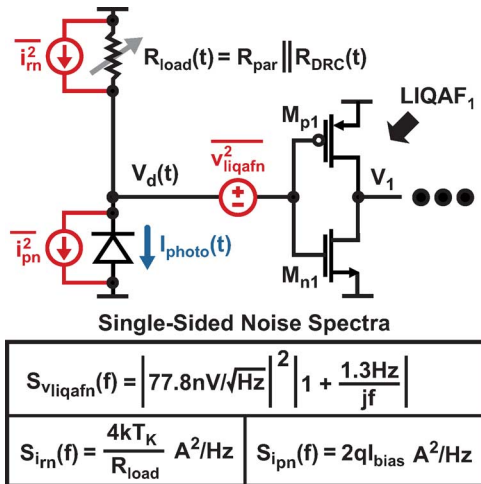


Fig. 14. Key front-end noise sources of proposed LDC.

decreasing value of R_{load} . For the photodiode in particular, note that its current is multiplied by R_{load} to form the voltage at node $V_d(t)$, and that reduction of R_{load} outweighs the increase in photodiode shot noise that occurs as I_{bias} is increased. Second, assuming $R_{par} = 10$ M Ω , the dominant noise source varies from R_{load} thermal noise at low I_{bias} to the LIQAF thermal and $1/f$ noise at high I_{bias} . While not shown, for the case where R_{par} is removed, the noise behavior is similar at high I_{bias} , but is dominated by photodiode shot noise at low I_{bias} . Third, we see that the LIQAF thermal and $1/f$ noise has only a minor impact for the assumed 0.5–5-Hz integration bandwidth, such that

correlated double sampling or chopping techniques [15] are unnecessary. Further on this issue, it should be noted that the inverter-based LNA provided by the LIQAF quantizer has a very long effective transistor length since it consists of the series cascade of multiple CMOS devices, which aids in reducing the impact of $1/f$ noise.

Finally, inspection of Fig. 15(c) leads to several key observations regarding the front-end SNR. First, the front-end SNR increases with increasing I_{bias} , with a minimum SNR of approximately 34 dB achieved with $I_{bias} = 4$ nA. Second, SNR could be improved by removing R_{par} , but at the cost of either reduced range of I_{bias} or of significantly more area in the DRC. Of course, the achievable front-end SNR will be influenced by PVT variations, with the primary influence being variations in the LIQAF quantizer which lead to variations in the bias voltage on the photodiode (which is set through the LDC feedback such that the LIQAF quantizer is centered in its fine quantization region) and variations in the bias current through the LIQAF (due to its inverter-based implementation). The former issue leads to a shift in the supported I_{bias} range, though adjustment of R_{par} can be used to maintain LDC sensitivity (i.e., minimum I_{bias}). The latter issue leads to increased/decreased input-referred thermal noise of the LIQAF LNA for lower/higher LIQAF bias current, respectively.

C. Impact of LIQAF and $\Delta\Sigma$ Quantization Noise

In a well-designed LDC, the front-end noise sources set the SNR as calculated in the previous subsection. Here, we will show that the proposed LDC architecture largely maintains the

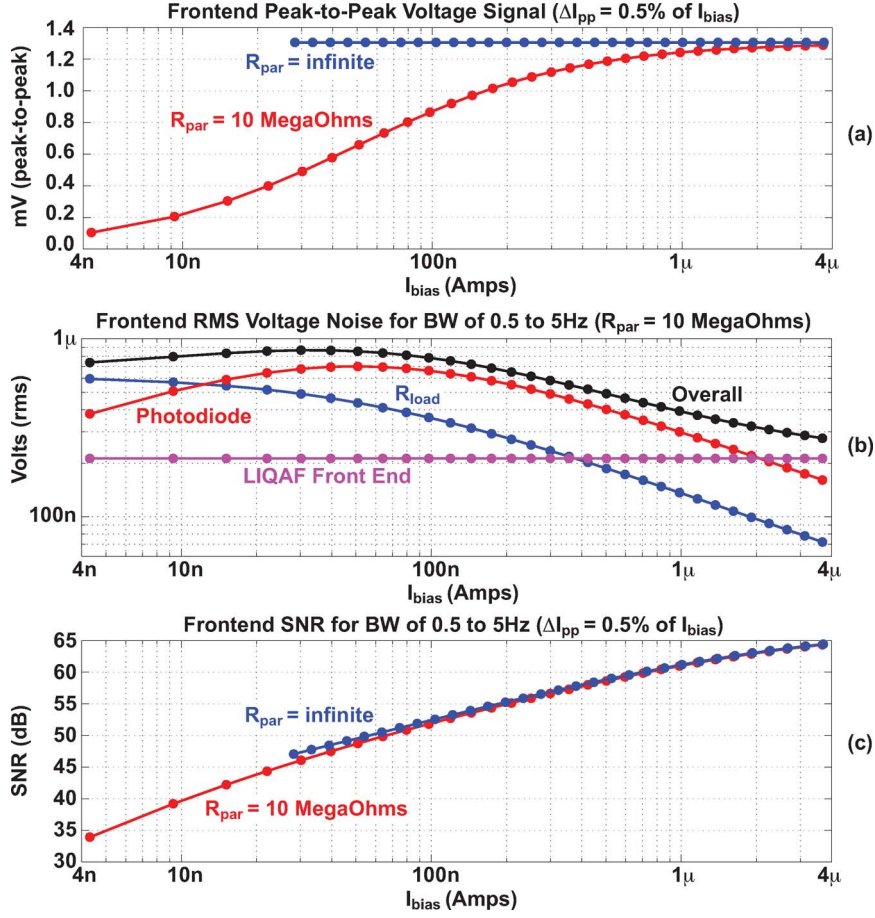


Fig. 15. Calculated plots for front-end signals referred to node $V_d(t)$ as a function of I_{bias} assuming the signal given in (2) with $\Delta I_{pp} = 0.5\%$ of I_{bias} and noise given in Fig. 14: (a) peak-to-peak voltage swing, (b) noise for the case where $R_{\text{par}} = 10 \text{ M}\Omega$, and (c) front-end SNR.

front-end SNR despite the presence of quantization noise that is introduced by the LIQAF quantizer and $\Delta\Sigma$ dithering of DRC resistor values. As such, we affirm that using the LIQAF quantizer and DRC is theoretically sound for achieving a high-performance LDC.

Fig. 16 provides a block diagram of the overall LDC along with its key noise sources. In addition to the front-end noise sources already discussed, quantization noise of the LIQAF quantizer and DRC digital $\Delta\Sigma$ modulator are also included and are denoted as q_{liqaf}^2 and q_{sd}^2 , respectively. In contrast to the continuous-time (CT) front-end noise sources, the quantization noise sources are discrete-time (DT) in nature. To model the impact of passing between CT and DT domains, the operations of sampling and reconstruction are included in the figure as scale factors $1/T_{\text{clk}}$ and T_{clk} , respectively [16]. Here, T_{clk} corresponds to the period of the 32-kHz clock used by the LDC.

In order to simplify the noise analysis, we observe that the poles of the front-end filter and LIQAF quantizer should be higher than the closed-loop bandwidth of the LDC in order to assure robust stability of its dynamics. As such, for frequencies within the LDC bandwidth, which is $< 5 \text{ Hz}$, it is a reasonable approximation to ignore the front-end filter and LIQAF quantizer poles. In doing so, the various noise sources of the LDC become separated by simple gain blocks as shown in the top

portion of Fig. 17. Therefore, we can refer all noise sources to the front-end of the LDC as shown in the bottom portion of the figure. Note that the extra $1/T_{\text{clk}}$ scale factor present in both spectral density calculations is required due to the translation from DT to CT when referring the quantization noise sources to the front-end [16].

Calculation of the single-sided spectral density for the first-order $\Delta\Sigma$ quantization noise [16] is given by

$$S_{q_{\text{ds}}}(f) = 2 \frac{1}{12} |1 - z^{-1}|^2$$

where

$$z = e^{j2\pi f T_{\text{clk}}}. \quad (3)$$

The above equation assumes well-scrambled quantization noise, but this assumption is often violated by first-order modulators. Instead, their noise spectra often contains significant spurious tones that vary in frequency according to the input of the modulator. In practice, detailed behavioral simulations must be utilized in order to estimate the actual noise spectra of the first-order $\Delta\Sigma$ modulator under different operating conditions. However, for the sake of simplicity, we will use (3) for the analysis to follow.

Calculation of the single-sided spectral density of the cascaded LIQAF quantization noise, $S_{q_{\text{liqaf}}}(f)$, is complicated by its nonuniform characteristic. Fig. 18 shows equivalent circuit

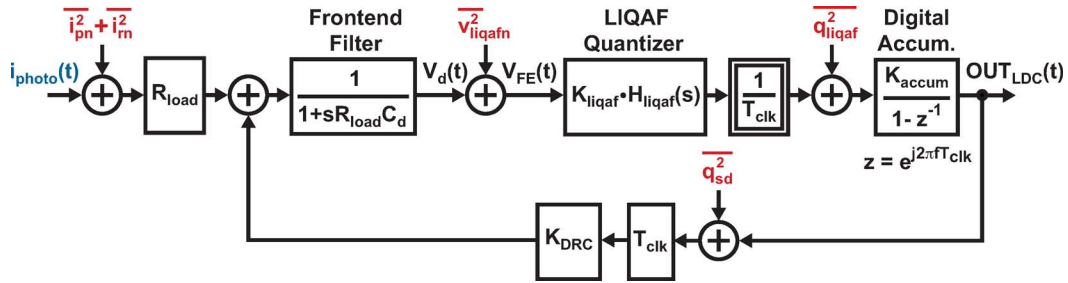


Fig. 16. Simplified block diagram of proposed LDC including key noise sources.

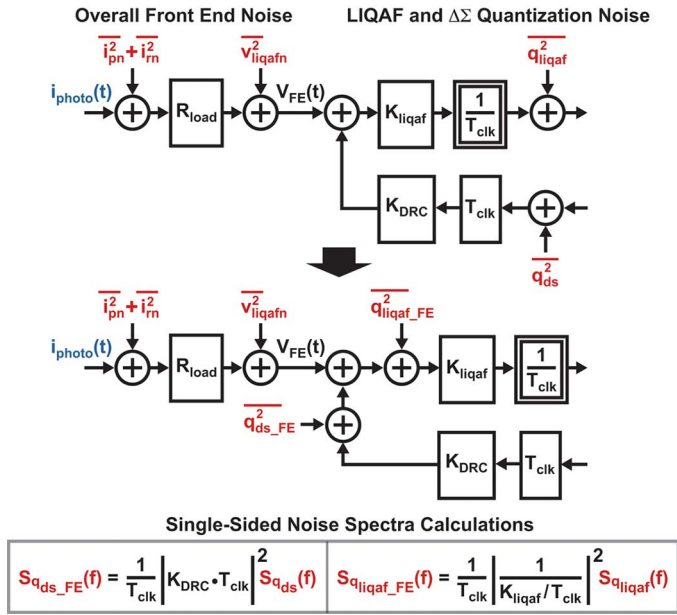


Fig. 17. Front-end referral of LIQAF and $\Delta\Sigma$ quantization noise.

diagrams for the front-end and cascaded LIQAF quantizer under fine and medium quantization regions assumed for low and high I_{bias} operation, respectively. In the figure, note that C_d represents the overall capacitance at node $V_d(t)$. It is assumed that, under normal steady-state operating conditions, the voltage deviation at node $V_d(t)$ is too small to activate the coarse quantization region. Movement from fine to medium quantization regions as a function of I_{bias} is due to the relative change in signal swing at node $V_d(t)$ as a function of I_{bias} , as shown in Fig. 15(a), and also due to increased influence of the DRC $\Delta\Sigma$ quantization noise since the front-end bandwidth increases as R_{load} decreases. Measurements of the prototype validate the correspondence between quantization region operation and the value of I_{bias} for the assumed $I_{photo}(t)$ amplitude of $\Delta I_{pp} = 0.5\%$ of I_{bias} .

Due to the change in quantization region as a function of I_{bias} , the dc gain K_{liqaf} , transfer function $H_{liqaf}(f)$, and spectral density of the quantization noise $S_{q_{liqaf}}(f)$ of the LIQAF quantizer also vary with I_{bias} , as indicated in the figure. In particular, note that the value of K_{liqaf} reduces by nearly half in going from low to high I_{bias} conditions, which somewhat offsets the factor of two increase in DRC gain occurring over the same conditions.

The culmination of our quantization noise analysis is a summary of its influence on the noise and SNR of the LDC

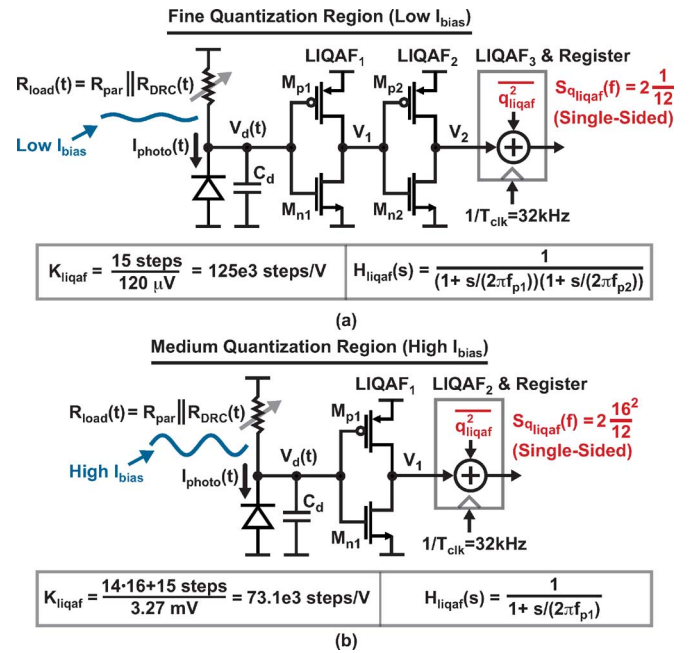


Fig. 18. Modeling of LIQAF as a function of I_{bias} conditions. (a) Small variation of $V_d(t)$ with low I_{bias} exercises quantization behavior of third LIQAF stage to achieve fine quantization levels. (b) Larger variation of $V_d(t)$ with high I_{bias} exercises quantization behavior of second LIQAF stage to activate medium quantization levels.

as depicted in Fig. 19. Here, we see the relative influence of the $\Delta\Sigma$ and LIQAF quantization noise compared with the overall front-end noise that was shown in Fig. 15. As revealed by part (a) of the figure, the influence of the $\Delta\Sigma$ noise within the 0.5–5-Hz integration bandwidth is relatively minor assuming (3) is valid (i.e., the DRC $\Delta\Sigma$ quantization noise is well scrambled). In contrast, the influence of the LIQAF quantization noise depends on whether it is operating in its fine or medium quantization region. In the case of low I_{bias} , the fine quantization region is active such that the LIQAF quantization noise has very little impact. However, in the case of high I_{bias} , the medium region is active and the resulting LIQAF quantization noise becomes the dominant noise source. As revealed by Fig. 19(b), these observations are confirmed by noting that the SNR plot under low I_{bias} conditions (with fine quantization noise assumed) is nearly the same as that obtained for the front-end noise shown in Fig. 15(c), whereas the SNR plot under high I_{bias} conditions (with medium quantization noise assumed) reveals somewhat degraded performance.

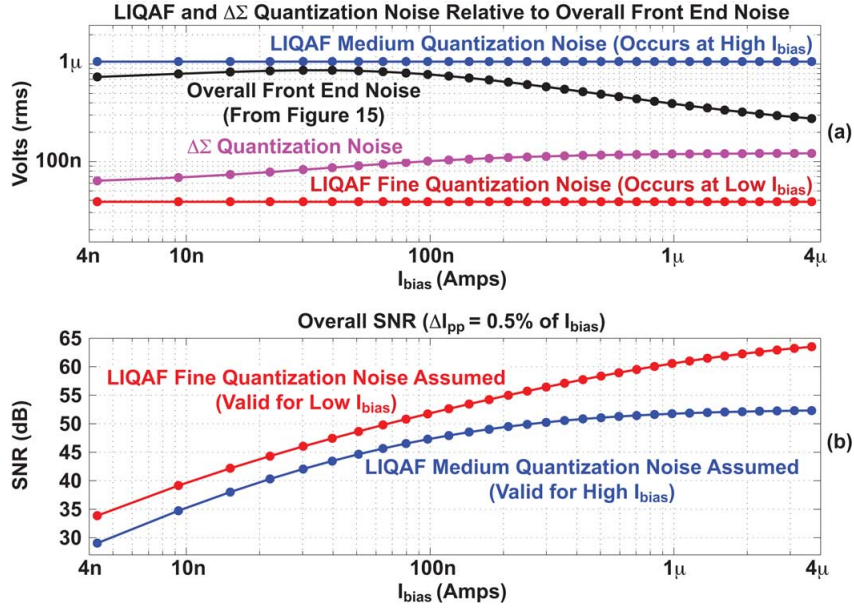


Fig. 19. Calculated plots for front-end referral of LIQAF and $\Delta\Sigma$ quantization noise. (a) Comparison with overall front-end noise. (b) Overall SNR versus I_{bias} for $\Delta I_{pp} = 0.5\%$ of I_{bias} under LIQAF fine and medium quantization region assumptions.

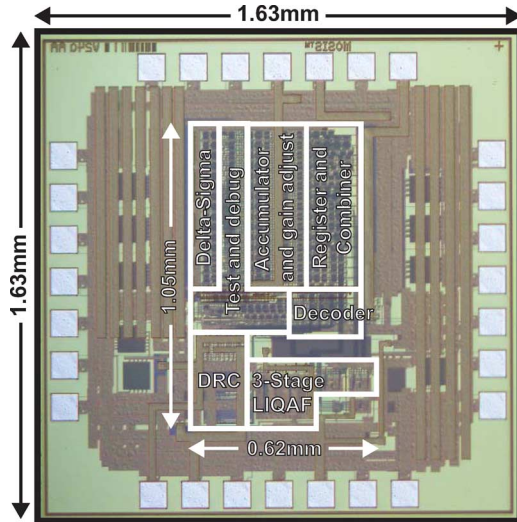


Fig. 20. Die photograph of LDC prototype IC in 180-nm CMOS.

TABLE I
MEASURED CURRENT CONSUMPTION OF KEY BLOCKS
WITHIN THE LDC AT 0.5-V SUPPLY VOLTAGE

Circuit Component	Current consumption at $I_{bias} = 4\text{nA}$	Current consumption at $I_{bias} = 3500\text{nA}$
LIQAF (3 Stages)	165nA	165nA
DRC	100nA	3.5 μ A
Digital Circuits	3.1 μ A	3.1 μ A
Total	<3.5μA	<7μA

In summary, comparison of the SNR plots in Figs. 15(c) and 19(b) reveal that the proposed LDC will achieve its front-end noise limit at low values of I_{bias} , and will lose about 13 dB in SNR at high values of I_{bias} . Since the key specification is the minimum SNR, which occurs at low I_{bias} under the assumptions

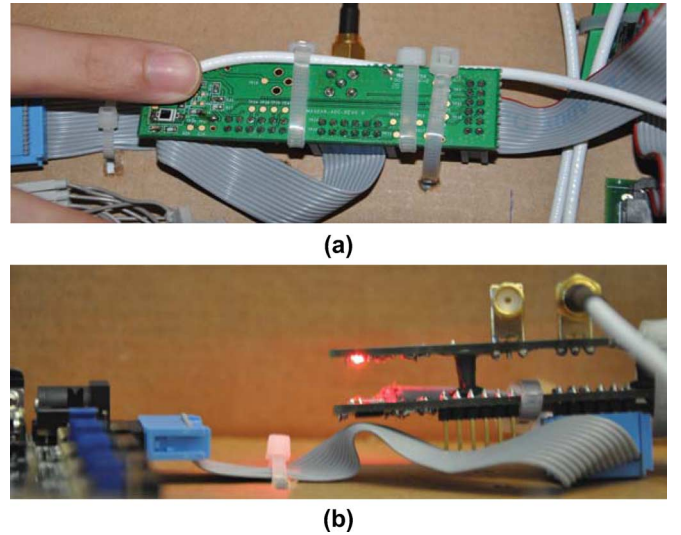


Fig. 21. Physical test setup for (a) using ambient light through a finger to measure heart rate and (b) using a 0.5%, 1%, and 2% peak-to-peak modulated LED to stimulate the photodiode at different bias currents and modulation frequencies.

of the above analysis, we see that the proposed approach of using the LIQAF nonuniform quantizer and DRC theoretically maintains the sensitivity set by the front-end noise sources and offers the advantages of a wide dynamic range and highly digital implementation.

V. MEASURED RESULTS

Fig. 20 displays a die photograph of the proposed LDC, which is fabricated in a 180-nm CMOS process. As indicated in the figure, the overall die area is 2.7 mm² (i.e., 1.63 mm \times 1.63 mm), and the active area is 0.65 mm² (i.e., 1.05 mm \times 0.62 mm). Interestingly, we see that the active die area is dominated by digital blocks, with the analog DRC and three-stage

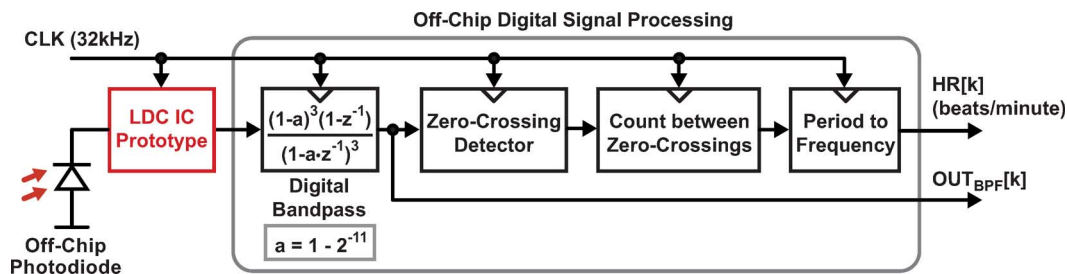


Fig. 22. Block diagram of test setup with digital signal processing used for calculation of heart rate.

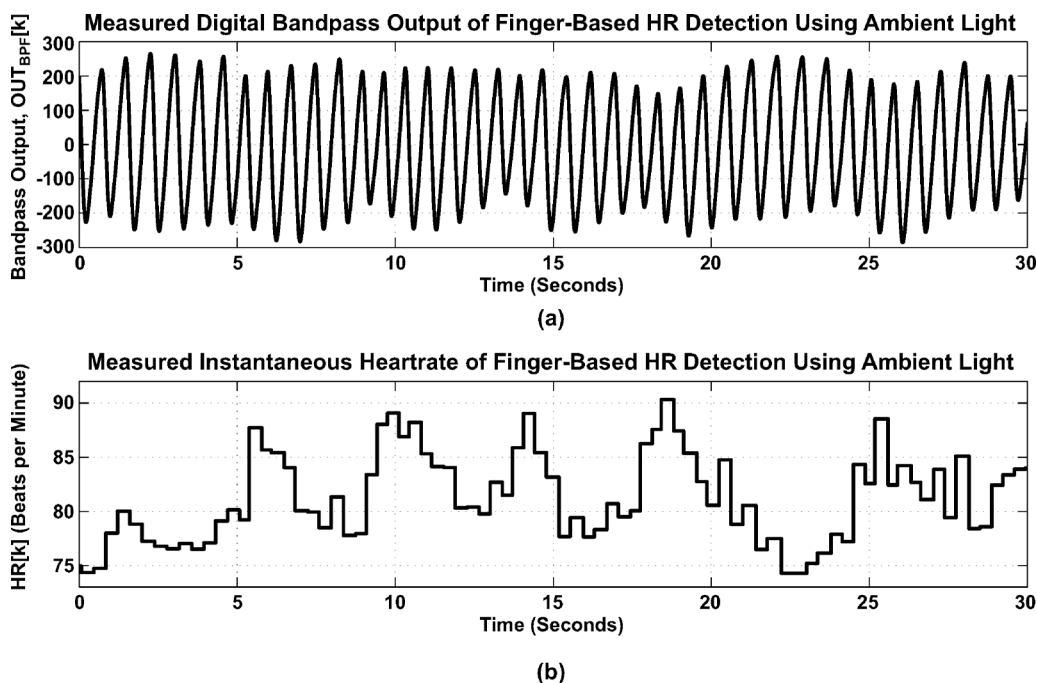


Fig. 23. Measured results using ambient light through a finger: (a) output of digital bandpass and (b) instantaneous HR frequency.

LIQAF quantizer consuming less than one third of the active area. Note that the LDC prototype achieves less than 5-Hz closed-loop bandwidth with no off-chip components other than the external photodiode and bypass capacitors for the supply voltage.

Measured current consumption of the IC prototype varies with the photodiode bias current, with the maximum current occurring at maximum I_{bias} . As shown in Table I, measured current consumption of the IC at 0.5-V supply voltage is $< 7 \mu\text{A}$ (excluding output data drivers) across the I_{bias} operation limits of 4 nA/3.5 μA , which corresponds to power consumption of $< 4 \mu\text{W}$. Note that operation of the LDC was also confirmed through measurements at 0.4- and 0.6-V supply voltages. Measured IC current consumption (excluding output data drivers) at 0.4-V supply was 2.9 μA /5.3 μA across the I_{bias} operation limits of 4 nA/2.5 μA , and at 0.6-V supply was 4.6 μA /8.8 μA across the I_{bias} operation limits of 4 nA/4.3 μA .

Fig. 21 shows the test setup used to characterize the LDC performance. The board contains two parallel channels (i.e., two photodiodes and two LDC ICs), a clock source, voltage regulators (to minimize 50 Hz power supply noise), and connectors for voltage supplies, digital controls, and test data. The photodiode (part number SFH 2430 from OSROM Opto Semiconductors)

contributes 1 nF of capacitance to the LDC front-end filter. The clock source has a frequency of 2 MHz in order to facilitate serialization of test signals and is divided down by a factor of 64 internal to the IC in order to achieve an LDC clock frequency of $1/T_{clk} = 31.25 \text{ kHz}$. Fig. 21(a) indicates the test case in which a finger is placed on top of the photodiode in order to assess the ability of the system to sense heart rate using only ambient light [17]. One can see the photodiode of the other channel in the figure, which was not used in the set of experiments discussed in this paper. Fig. 21(b) indicates the test case in which a separate board containing an LED is mounted on top of the IC test board in order to characterize the sensitivity and dynamic range of the LDC. When performing such characterization, the setup is placed in a light-shielded environment and the LED current is modulated with a sine wave such that the photodiode current has $\Delta I_{pp} = 0.5\%$, 1% and 2% of I_{bias} with both I_{bias} and the sine wave frequency being varied across the operating range of the LDC. The photodiode current is measured for this test by examining the voltage across a 10 k Ω resistor that is placed in series with the photodiode.

In order to extract the LED modulation frequency or heart rate from the LDC output, external digital signal processing is applied as shown in Fig. 22. The heart-rate detection algorithm

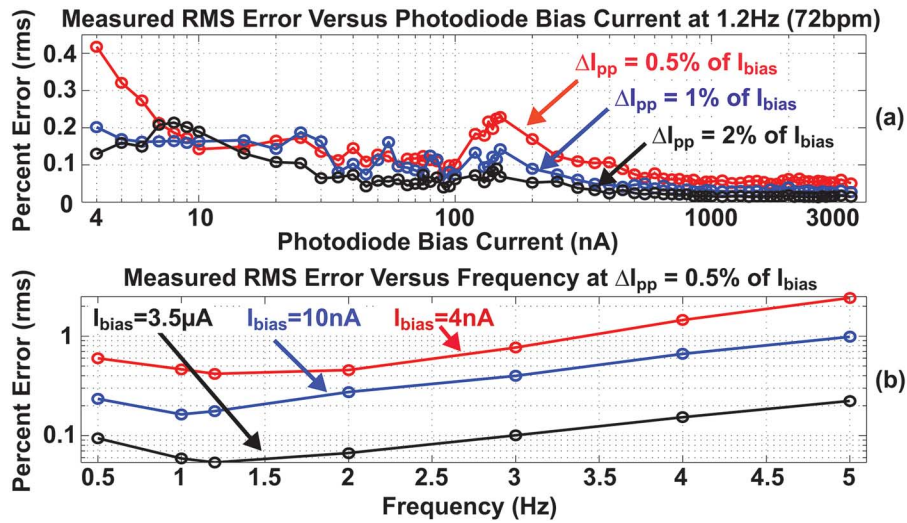


Fig. 24. Measured results using a sine wave modulated LED source. (a) RMS error versus photodiode bias current. (b) RMS error versus modulation frequency.

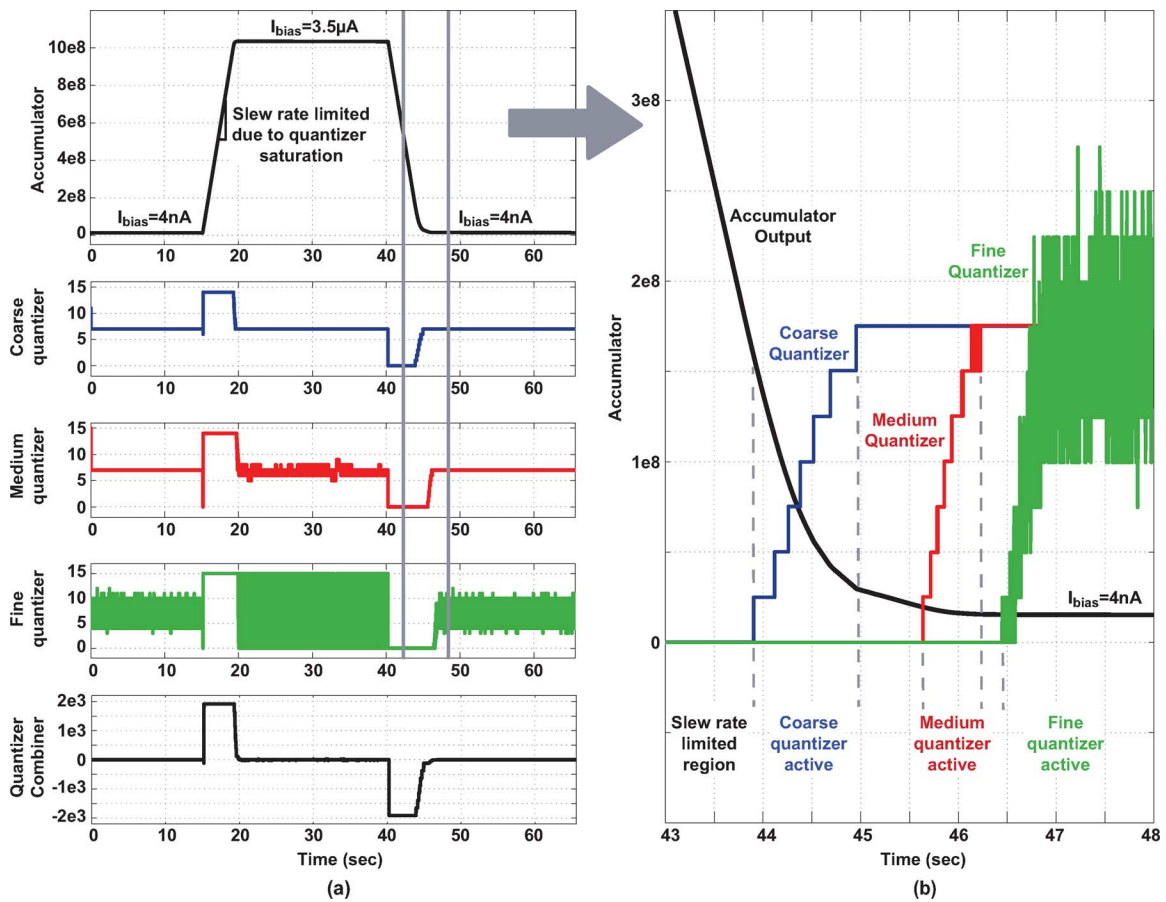


Fig. 25. Measured step response of accumulator, individual quantizer stages, and quantizer combiner outputs across full range of LDC. (a) Full view. (b) Zoomed-in view.

consists of a digital bandpass filter followed by edge detection and a digital counter which keeps track of times between edges. The LED modulation frequency or heart rate is then computed based on the measured times between consecutive rising edges as well as consecutive falling edges.

Given the above setup, Fig. 23 displays the measured results in the case where ambient light within an office environment

is used with a finger placed over the photodiode. For the plots shown, the measured photodiode bias current is $I_{bias} = 17$ nA. Fig. 23(a) shows the LDC output after it passes through the digital bandpass filter shown in Fig. 22, and Fig. 23(b) shows calculated instantaneous heart rate. One should note that the estimated heart rate is on a per-beat basis with no additional averaging applied across beats. The variation in the heart rate would

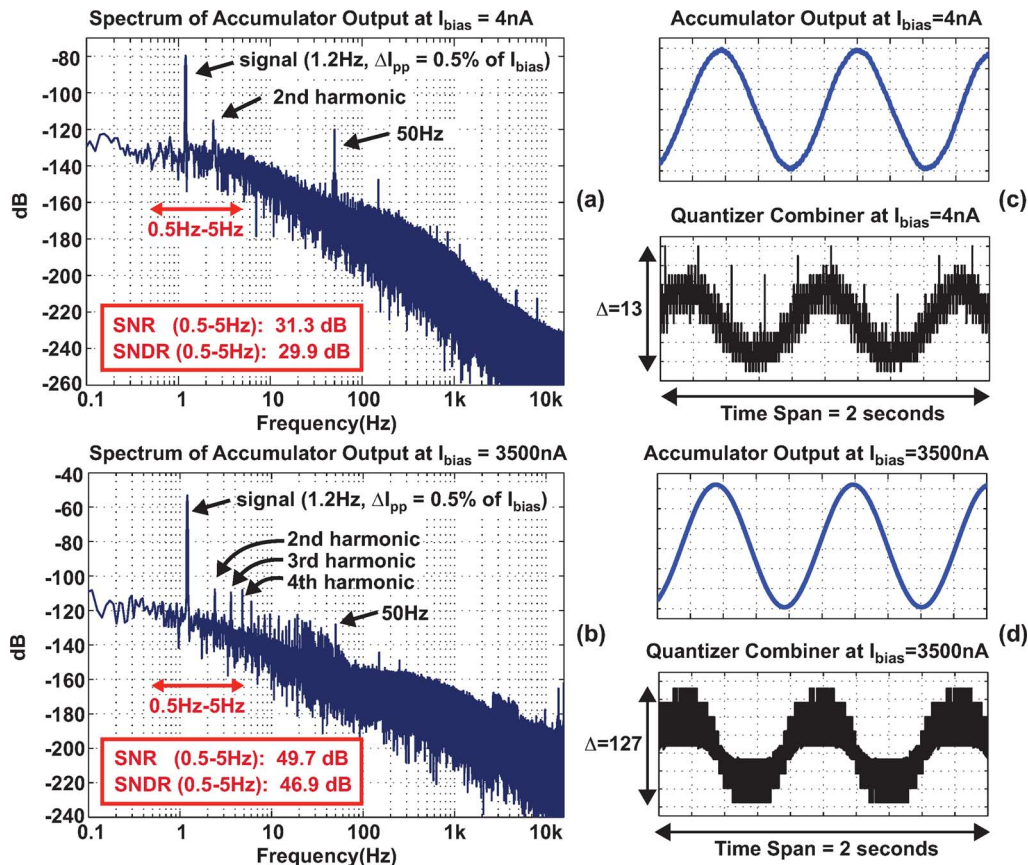


Fig. 26. Measured spectrum of LDC output for approximately 60 seconds of data sampled at 31.25 kHz with $\Delta I_{pp} = 0.5\%$ of I_{bias} at 1.2 Hz (72 bpm) frequency under (a) low I_{bias} of 4 nA for the photodiode and (b) high I_{bias} of 3.5 μA for the photodiode. (c), (d) Zoomed-in time-domain view of measured accumulator and quantizer combiner outputs corresponding to the spectra in (a) and (b), respectively.

be reduced if such averaging were employed. When considering the use of ambient light across a wider range of conditions, we note that indoor versus outdoor light varies by three orders of magnitude in intensity [18], which is a reasonably close match to the I_{bias} range supported by the proposed LDC. However, full benchmarking of ambient light-based HR detection performance was beyond the scope of this work.

Fig. 24 displays measured results in the case where the external, modulated LED is used to characterize the LDC over its full range of photodetector bias current and modulation frequency by sensing rms error of the calculated modulation frequency, which serves as a proxy for heart rate. Fig. 24(a) demonstrates that the rms error versus I_{bias} is less than 0.45% across the entire I_{bias} range from 4 nA to 3.5 μA assuming an LED modulation frequency of 1.2 Hz. As such, a minimum sensitivity of $I_{bias} = 4$ nA and dynamic range of $20 \log(3.5 \mu A / 4 \text{ nA}) = 58.8$ dB is achieved. Fig. 24(b) displays rms error versus modulation frequency with $I_{bias} = 4$ nA, 10 nA, and 3.5 μA . Note that the worst case rms error of 2.5% occurs at the maximum frequency of 5 Hz (i.e., 300 bpm) due to the fact that the small period at this 5-Hz frequency leads to a larger *percentage* error. The high-frequency performance could also be somewhat improved if the bandpass filter within the digital signal processing block was designed to be adaptive in its center frequency setting.

Fig. 25 shows the measured response of the accumulator, individual quantizer stages, and the overall quantizer combiner

for a step change in LED light intensity across the full dynamic range of the LDC. The response is slew-rate limited due to saturation of the quantizer. The slight glitch seen at the beginning of the first step is due to the external function generator that was used to drive the LED current. Note that the plot reveals that the fine quantizer levels are active at low I_{bias} , and the medium quantizer levels are active at high I_{bias} . Since no LED modulation is occurring in this test, the increase in quantizer activity at higher I_{bias} is attributed to the higher impact of the DRC $\Delta\Sigma$ quantization noise due to the increased front-end filter bandwidth (i.e., reduced value of R_{load}).

Measured spectra of the LDC output (i.e., accumulator output) for $\Delta I_{pp} = 0.5\%$ of I_{bias} are shown in Fig. 26 under low and high I_{bias} conditions of 4 nA and 3.5 μA , respectively. Measured SNR is obtained from the spectral plots assuming 0.5-5-Hz integration bandwidth and should be compared with the calculated SNR plots shown in Fig. 19(b). As observed from this comparison, measured SNR is about 3 dB worse than theoretical calculations under low and high I_{bias} conditions. The measured SNDR values are close to their SNR counterparts, which indicates that the LDC feedback dynamics are approximately linear in behavior. Finally, the time domain plots of the quantizer combiner output shown in Fig. 26(c) and (d) confirm that the fine quantization region is active at low I_{bias} and the medium region is active at high I_{bias} .

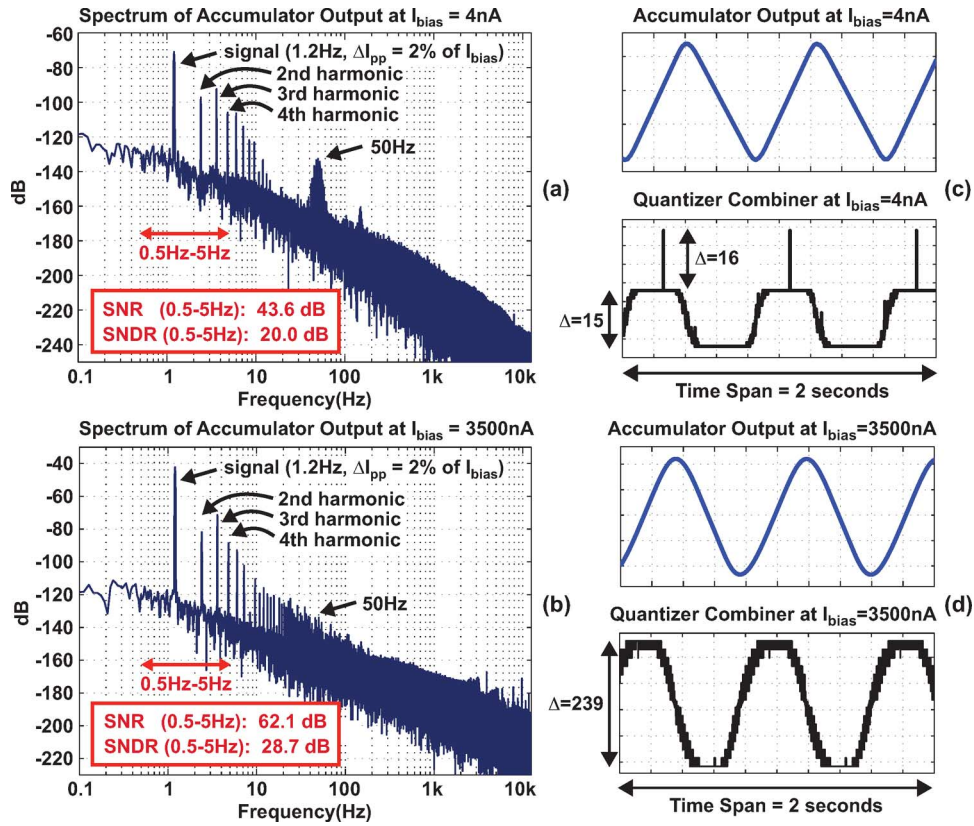


Fig. 27. Measured spectrum of LDC output for approximately 60 seconds of data sampled at 31.25 kHz with $\Delta I_{pp} = 2\%$ of I_{bias} at 1.2 Hz (72 bpm) frequency under (a) low I_{bias} of 4 nA for the photodiode and (b) high I_{bias} of 3.5 μ A for the photodiode. (c), (d) Zoomed-in time-domain view of measured accumulator and quantizer combiner outputs corresponding to the spectra in (a) and (b), respectively.

TABLE II
 COMPARISON WITH OTHER PUBLISHED WORK

Ref	Process	Power (μ W)	V_{supply} (Volts)	Photodetector I_{bias} Sensitivity	Photodetector I_{bias} Range	Application
[10]	0.35u CMOS	600	2.5	100nA	54.6dB	Heartrate
[11]	0.35u CMOS	4500	3	Not Reported	40dB	Heartrate
[13]	1.5u BiCMOS	400	5	50nA (typical)	Not Reported	Oximetry
This Work	0.18u CMOS	<4	0.5	4nA	58dB	Heartrate

To see the impact of higher modulation amplitude, measured spectra of the LDC output for $\Delta I_{pp} = 2\%$ of I_{bias} are shown in Fig. 27 under the same low and high I_{bias} conditions as in Fig. 26. Here, we see that measured SNR improves by approximately 12 dB due to the fact that the signal for $\Delta I_{pp} = 2\%$ of I_{bias} is 12 dB higher than for $\Delta I_{pp} = 0.5\%$ of I_{bias} . However, the time-domain plots shown in Fig. 27(c) and (d) reveal saturation behavior in the quantizer and corresponding slewing behavior in the accumulator output such that SNDR is significantly degraded. As revealed by the rms error measurements results shown in Fig. 24, the improved SNR at higher modulation amplitude generally leads to better performance despite the nonlinear behavior of the nonuniform quantizer.

Finally, Table II compares the performance of the proposed LDC to other recent work. As shown by the table, the prototype presented in this paper achieves better sensitivity and range than other published work while also operating at significantly lower supply voltage and power dissipation.

VI. CONCLUSION

This paper presented a 0.5-V CMOS LDC that supports a wide photodiode bias current range of 4 nA to 3.5 μ A with less than 4 μ W of power consumption. Assuming a 1.2-Hz modulated photodiode current having 0.5% peak-to-peak amplitude relative to I_{bias} , better than 30 dB SNR is achieved at the low and high end of the I_{bias} range for an integration bandwidth spanning 0.5 to 5 Hz. Off-chip digital signal processing of the LDC output is used to calculate instantaneous period jitter (a proxy for instantaneous heart rate), which was measured to be less than 0.45% (rms) of the period across the full I_{bias} range. In addition, the excellent sensitivity of the LDC allowed detection of the heart-rate signal from a finger pressed against the off-chip photodiode using only ambient light.

Key circuit components of the LDC include a wide range logarithmic DRC utilizing digital multibit $\Delta\Sigma$ modulation to achieve fine resolution, and a nonuniform quantizer based on a

cascaded, laddered inverter quantizer (LIQAF) which also acts as a low-noise front-end amplifier and filter. The DRC, combined with a parallel resistor R_{par} , allows nearly three orders of magnitude in range for I_{bias} with only a 5-b design. The LIQAF-based quantizer provides a low-noise analog-to-digital interface with low power and low analog design complexity. As revealed by detailed calculations which assume I_{photo} amplitude of $\Delta I_{\text{pp}} = 0.5\%$ of I_{bias} , the theoretical worst case LDC SNR performance under low I_{bias} conditions is limited by front-end noise rather than quantization noise from the DRC or LIQAF-based quantizer.

Due to the 0.5-V supply voltage and extremely low power consumption of $< 4 \mu\text{W}$, the proposed LDC may offer the possibility of enabling compact solar-powered heart-rate sensors that are embedded in rings [19] or other wearable devices. Since the excellent sensitivity of the LDC allows ambient light to be used, such devices could potentially operate without LED light sources and be used to sample heart rate when appropriate ambient light levels are present.

ACKNOWLEDGMENT

The authors would like to thank Berkeley Design Automation for use of their AFS simulator.

REFERENCES

- [1] W. Saadeh, T. Tekeste, and M. Perrott, "A $> 89\%$ efficient LED driver with 0.5 V supply voltage for applications requiring low average current," in *Proc. IEEE Asian Solid-State Circuits Conf.*, Nov. 2013.
- [2] J. G. Webster, *Design of Pulse Oximeters*. New York, NY, USA: Taylor and Francis, 1997.
- [3] C.-C. Hsu and J.-T. Wu, "A highly linear 125-MHz CMOS switched-resistor programmable-gain amplifier," *IEEE J. Solid-State Circuits*, vol. 38, no. 10, pp. 1663–1670, Oct. 2003.
- [4] M. Alhawari, N. Albelooshi, and M. Perrott, "A 0.5 V $< 4 \mu\text{W}$ CMOS photoplethysmographic heart-rate sensor IC based on a non-uniform quantizer," in *IEEE Int. Solid-State Circuits Conf. Dig. Tech. Paper*, Feb. 2013, pp. 384–385.
- [5] A. Karanicolas, "A 2.7-V 900-MHz CMOS LNA and mixer," *IEEE J. Solid-State Circuits*, vol. 31, no. 12, pp. 1939–1944, Dec. 1996.
- [6] F. de Jager, "Delta modulation, a method of PCM transmission using a 1-unit code," *Phillips Res. Rep.*, pp. 442–466, Dec. 1952.
- [7] J. Abate, "Linear and adaptive delta modulation," *Proc. IEEE*, vol. 55, no. 3, pp. 298–308, Mar. 1967.
- [8] M. W. Hauser, "Principles of oversampling A/D conversion," *J. Audio Eng. Soc.*, vol. 39, no. 1/2, pp. 3–26, 1991.
- [9] W. Kester and J. Bryant, "Sigma-Delta converters," in *Data Conversion Handbook*, W. Kester, Ed. Burlington, MA, USA: Newnes, 2005.
- [10] A. Wong, K.-P. Pun, Y.-T. Zhang, and K. Leung, "A low-power CMOS front-end for photoplethysmographic signal acquisition with robust DC photocurrent rejection," *IEEE Trans. Biomed. Circuits Syst.*, vol. 2, no. 4, pp. 280–288, Dec. 2008.
- [11] A. Wong, K.-P. Pun, Y.-T. Zhang, and K. Hung, "A near-infrared heart rate measurement IC with very low cutoff frequency using current steering technique," *IEEE Trans. Circuits Syst. I, Reg. Papers*, vol. 52, no. 12, pp. 2642–2647, Dec. 2005.
- [12] K. Phang and D. Johns, "A CMOS optical preamplifier for wireless infrared communications," *IEEE Trans. Circuits Syst. II, Analog Digit. Signal Process.*, vol. 46, no. 7, pp. 852–859, Jul. 1999.
- [13] M. Tavakoli, L. Turicchia, and R. Sarpeshkar, "An ultra-low-power pulse oximeter implemented with an energy-efficient transimpedance amplifier," *IEEE Trans. Biomed. Circuits Syst.*, vol. 4, no. 1, pp. 27–38, Feb. 2010.
- [14] C. Thompson and S. Bernadas, "A digitally-corrected 20 b delta-sigma modulator," in *Proc. IEEE Int. Solid-State Circuits Conf.*, Feb. 1994, pp. 194–195.

- [15] C. Enz and G. Temes, "Circuit techniques for reducing the effects of opamp imperfections: Autozeroing, correlated double sampling, and chopper stabilization," *Proc. IEEE*, vol. 84, no. 11, pp. 1584–1614, Nov. 1996.
- [16] M. H. Perrott, M. D. Trott, and C. G. Sodini, "A modeling approach for $\Sigma\Delta$ fractional-N frequency synthesizers allowing straightforward noise analysis," *IEEE J. Solid State Circuits*, vol. 37, no. 8, pp. 1028–1038, Aug. 2002.
- [17] W. Verkruyssen, L. Svaasand, and J. Nelson, "Remote plethysmographic imaging using ambient light," *Opt. Exp.*, vol. 16, pp. 21434–21445, Dec. 2008.
- [18] R. Vullers, R. Van Schaijk, H. Visser, J. Penders, and C. Van Hoof, "Energy harvesting for autonomous wireless sensor networks," *IEEE Solid-State Circuits Mag.*, pp. 29–38, 2010.
- [19] H. Asada, P. Shaltis, A. Reisner, S. Rhee, and R. Hutchinson, "Mobile monitoring with wearable photoplethysmographic biosensors," *IEEE Eng. Med. Biol. Mag.*, vol. 22, pp. 28–40, May 2003.



Mohammad Alhawari received the B.S. degree in electronics engineering from Yarmouk University, Jordan, in 2008, and the M.S. degree in microsystems engineering from Masdar Institute of Science and Technology, Abu Dhabi, UAE, in 2012. He is currently working toward the Ph.D. degree at Khalifa University, Abu Dhabi, UAE.

His M.S. research at Masdar focused on low-power, mixed-signal integrated circuit design which involved schematic design, simulation, layout, and verification of an ultra-low-power heart-rate sensor. From 2008 to 2010, he was with YOUNIVATE Company in Jordan as a Hardware and PCB designer. His current research focuses on low-power, mixed-signal circuits for energy-harvesting applications.



Nadya A. Albelooshi received the B.S. degree in information technology computer system engineering major from United Arab Emirates University, Al Ain, UAE, in 2008, and the M.S. degree in microsystems engineering from Masdar Institute of Science and Technology, Abu Dhabi, UAE, in 2012.

Her M.S. research at Masdar Institute of Science and Technology involved designing, modeling, analyzing, simulating, and verifying an efficient heart rate estimation algorithm and also achieving an ultra-low power digital signal processing implementation for the algorithm for wearable heart rate monitoring applications. From 2008 to 2010, she was an IT Services Coordinator with Sheikh Saqr Program for Government Excellence in Ras Al-Khaimah. She is currently with Abu Dhabi Company for Onshore Oil Operations (ADCO), Abu Dhabi, UAE.



Michael H. Perrott (SM'09) received the B.S. degree in electrical engineering from New Mexico State University, Las Cruces, NM, USA, in 1988, and the M.S. and Ph.D. degrees in electrical engineering and computer science from Massachusetts Institute of Technology, Cambridge, MA, USA, in 1992 and 1997, respectively.

From 1997 to 1998, he was with Hewlett-Packard Laboratories, Palo Alto, CA, USA, where he focused on high-speed circuit techniques for Sigma-Delta synthesizers. In 1999, he was a Visiting Assistant Professor with the Hong Kong University of Science and Technology. From 1999 to 2001, he was with Silicon Laboratories, Austin, TX, USA, where he developed circuit and signal processing techniques to achieve high-performance clock and data recovery circuits. He was an Assistant and then Associate Professor with the Department of Electrical Engineering and Computer Science, Massachusetts Institute of Technology, Cambridge, MA, USA, from 2001 to 2008. He was with SiTime Corporation from 2008 to 2010, where he developed key technology for MEMS-based oscillators. He was a Professor with the Masdar Institute of Science and Technology, Abu Dhabi, UAE, from 2011 to 2013, where he focused on low-power, mixed-signal circuits for health monitoring. He is currently with Silicon Laboratories, Nashua, NH, USA.